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CO₂ Laser and Micro-Fluidics

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1. Introduction

Microfluidic chips have attracted significant attention over the past decade due to their wide range of potential applications in the biomedical and chemical analysis field such as drug delivery, Point of care diagnostics (Jakeway et al, 2004), flow cytometry (Fu LM et al 2004; Chen & Wang, 2009; Lin et al, 2009), polymerize chain reaction (Suna et al, 2007; Sun & Kwok, 2006; Hsieh et al, 2009), electrophoresis (Fu et al, 2007, 2009) and many other applications.

Traditionally, silicon and glass are the predominant materials employed in the design of microfluidic systems. This was primarily due to their excellent chemical, physical, electrical and optical properties. But fabrication of a microfluidic device on these materials needs standard photolithography equipments such as Reactive Ion Etching (RIE) system which are very expensive and increases the production costs specially in single-use applications which are desired in order to avoid contamination.

In recent years application of polymeric materials for microfluidic device fabrication is becoming more and more important. Different methods for microfluidic fabrication on polymers such as hot embossing (Gerlach et al, 2002), injection molding (Rotting et al, 2002), soft lithography (Xia et al, 1998) and laser micromachining can be applied.

Different kind of lasers such as UV (Ball et al, 2000) and Infrared lasers is used for laser micromachining of polymers. In infrared regime, CO₂ laser has a predominant application due to its excellent absorption in polymers.

In this chapter, we will deal with application of a CO₂ laser in microfluidic device fabrication. The application of CO₂ laser for fabrication of a optofluidic device and application of a optofluidic device for CO₂ laser characterization is also presented.

2. Interaction of a CO₂ laser with polymers

Application of the CO₂ laser for microfluidic device fabrication was first proposed in 2002 by H. Klank et al (Klank et al, 2002).

CO₂ laser emits radiation with the wavelength of 10.6 micrometer. A CO₂ laser mostly interacts with a polymer, photo-thermally. When a CO₂ laser is irradiated on a polymer surface, it is strongly absorbed and raises the temperature of the polymer. The polymer is then melted, decomposed and leaving a void in a workpiece.

Different kind of polymers can be used for microfluidic applications by taking a choice care that the fluid in the device do not interact chemically with the device. However just some of the polymers can be machined with CO₂ laser. Most of the polymers leave contamination and soot when exposed to CO₂ laser irradiation. For example, polycarbonate (PC) leaves a brownish residue after exposing to the CO₂ laser.

Among different kind of polymers, poly methyl methacrylate (PMMA) is the most suitable polymer for CO₂ laser machining. When PMMA heats up by the CO₂ laser, after passing the glass temperature, the material turns into a rubbery material and by increasing the temperature, the chains are broken by depropagation process (Arisawa & Brill, 1997; Ferriol et al, 2003), and decompose with a non-charring process to it's MMA monomer which is volatile



Fig. 1 shows the decomposition process of PMMA polymer.

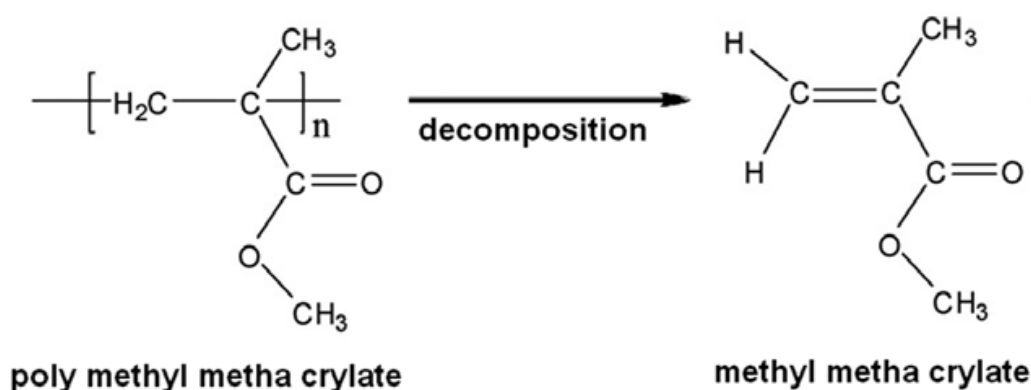


Fig. 1. Decomposition process of PMMA.

Decomposition of PMMA into volatile MMA monomers makes a hole in the workpiece. The shape and size of the hole, highly depends on the thermal properties of PMMA, focusing parameters, laser beam profile, exposure time and even exposure strategy. At the beginning of the exposure, the shape of the channel is very similar to the laser beam profile but as time goes up, the shape of the hole becomes more conical.

3. Fabrication of a channel on PMMA utilizing a CO₂ laser

Fabrication of a channel on the surface of PMMA can be performed by scanning a CO₂ laser over the surface of the workpiece. Commercial CO₂ engraving systems with laser powers about a few watts to a few tens of watts and scanning speeds from a few tens of mm/sec up to a few hundreds of mm/sec, are good choices for micro channel fabrication.

By scanning the PMMA surface with CO₂ laser, different channels and cavities can be fabricated. However, the ablated structures may be very rugged such that those can not be used for microfluidic structures with optical detection. Martin et al. reported that the roughness of the machined surfaces depends on the grade of the PMMA sheets. He reported roughness of 1.54 microns and 0.42 microns for two different grades of PMMA (Martin et al, 2003). Presence of the different roughness should probably be sought in the chemical additives of the different types of PMMA.

Cheng et. al. reported that the roughness of the machined channels can be treated by thermal annealing of the samples (Cheng et al 2004). Fig. 2. shows the surface of their work piece before and after annealing.

Hong et. al. also reported that the roughness of the microfluidic structures can be drastically reduced by out of focus machining of PMMA (Hong, et al, 2010).

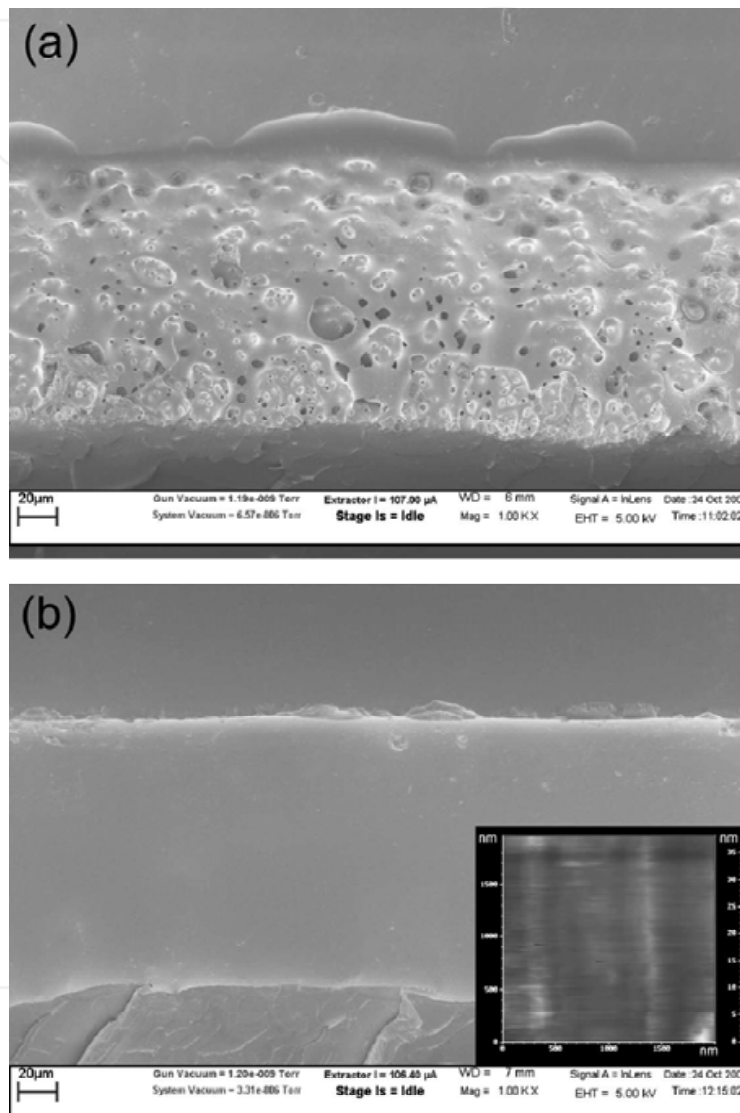


Fig. 2. The SEM pictures showing the rugged interior surface of the trench after laser machining (a) and smooth surface after thermal annealing (b). The AFM topography of the annealed surface is shown in the inset with full scale of 38 nm in the Z-axes. The viewing angle is perpendicular to the plane of the side wall (Cheng et al 2004) - Reproduced by permission of Elsevier under the license no. 283342005275.

PMMA micro fluidic structures can then be top covered by other polymers like PMMA or poly carbonate (PC) utilizing thermal-bonding process. Thermal bonding is a process of joining two materials by the mechanism of diffusion; and unity of the materials. This process is accomplished through the application of pressure at temperature higher than the glass temperature of the polymers.

In addition to fabrication of the holes, channels and cavities, CO₂ laser machining can be used to make some complicated structures, like bending holes. These structures can also be molded with other materials such as PDMS to get the negative of the PMMA structures. In the next section fabrication technique of the other complicated structure with 3D structure is presented.

4. Fabrication of a 3D Mixer with CO₂ laser machining of PMMA and PDMS molding

In this section we present application of a CO₂ laser for fabrication of a 3D mixer with bending cones (Riahi, 2012). Mixers are the elements in microfluidic and micro total analysis systems which are used for mixing two or more liquids in biological and chemical analyses. Mixers can be divided into the two categories, active and passive. In active mixers, an external actuation mechanism is used to mix liquids in a microfluidic chamber. In passive mixers, there is no energy consumption and the structure of these devices is simpler than that of active devices. Different schemes such as a Tesla structure (Hong et al, 2004), a T mixer (Hoe et al, 2004), a 3D serpentine (Liu et al, 2000) and twisted shapes (Bertsch et al, 2001) are also used in passive micro mixers.

The technique which is presented here is based on the application of the CO₂ laser for fabrication of some bending and straight cones on PMMA followed by PDMS molding. The designed mixer is shown in Fig. 3.

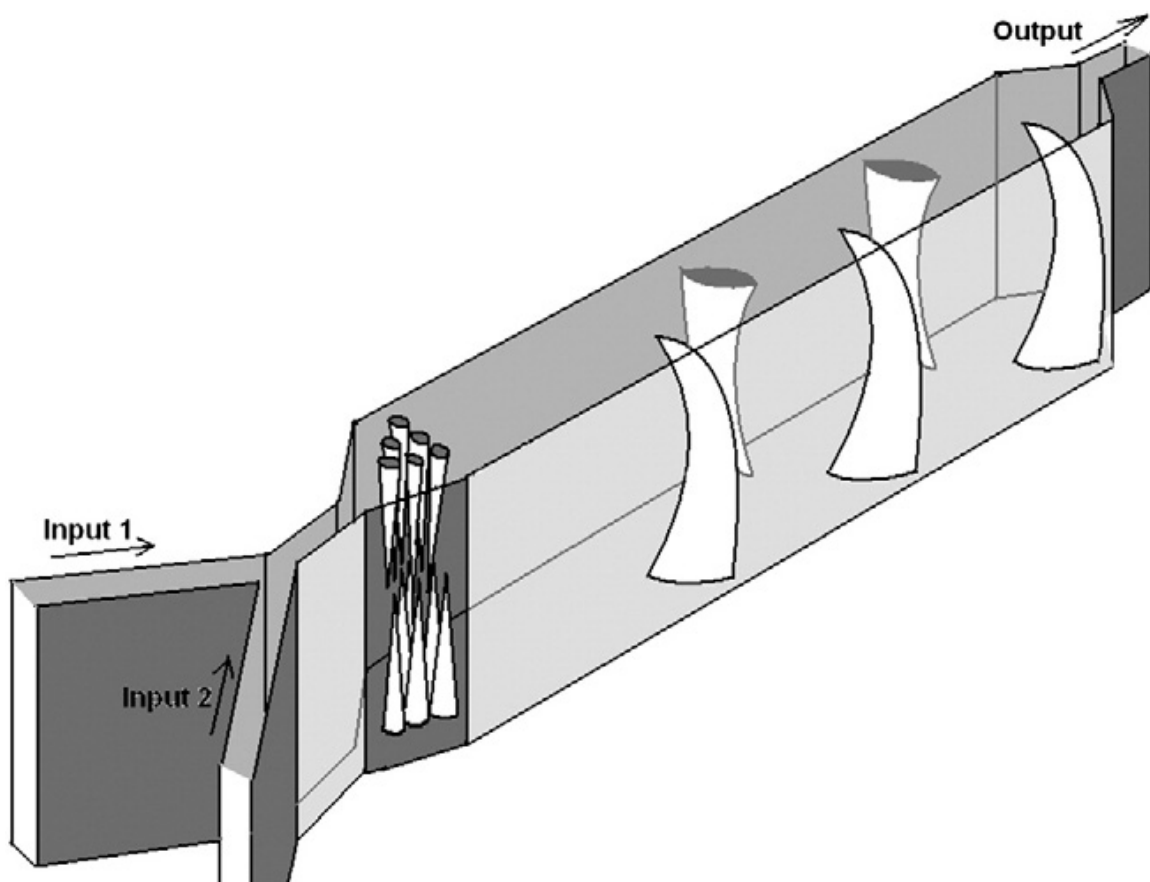


Fig. 3. Schematic of the designed 3D mixer (Riahi, 2012).

4.1 Fabrication of the bending cones

When a shape, is engraved in a raster scan mode by a CO2 laser engraving system on PMMA, the system scans a shape, row by row which each row has a certain overlap with a previous row. During the first row scan, a symmetrical V-shape channel is ablated on the PMMA surface. When the laser scans the subsequent rows, a small portion of the laser beam reflects from the wall of the channel produced by the previous scan to the bottom of the hole in the opposite side of the scanning direction as shown in Fig. 4a. After several scans, the reflected beam can ablate a considerable amount of PMMA material at the bottom of the hole at the opposite side of the scanning direction which can causes a bending shape in the structure (Fig. 4b).

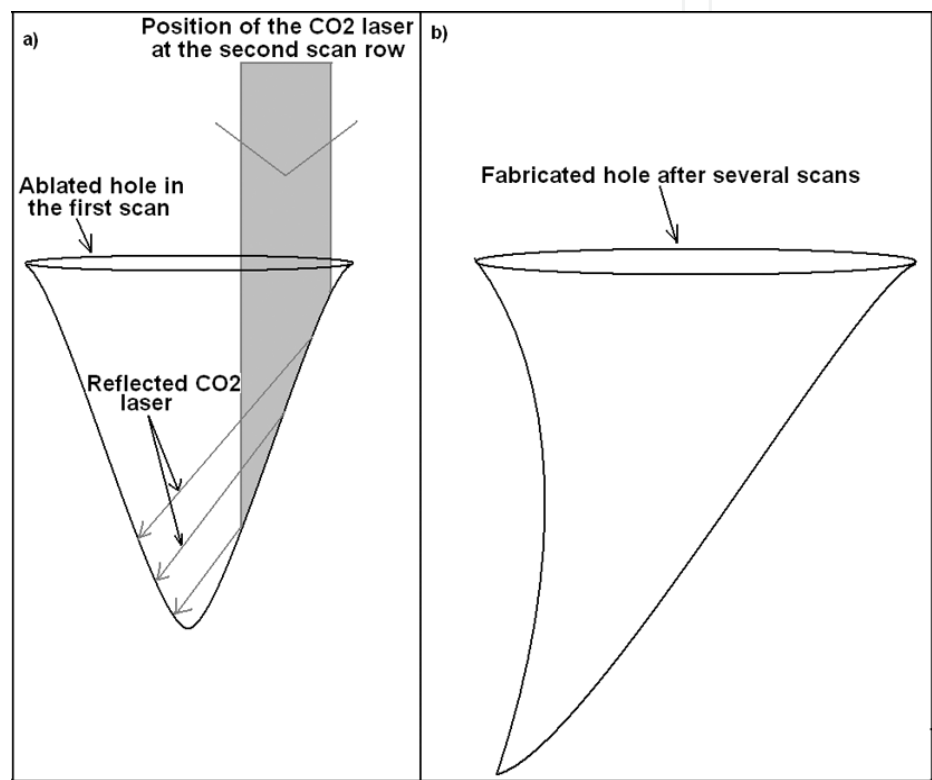


Fig. 4. Ablation of a PMMA hole with CO2 laser. a) Reflection of the laser from the walls of an ablated hole. b) The shape of the hole after several scans (Riahi, 2012).

It is found that the shape of the holes can be controlled by adjusting the scanning parameters such as resolution, power and scan speed. Some of the fabricated holes have very bent shapes and some are straight. Fig. 5 shows the ablated bending holes for different scan parameters.

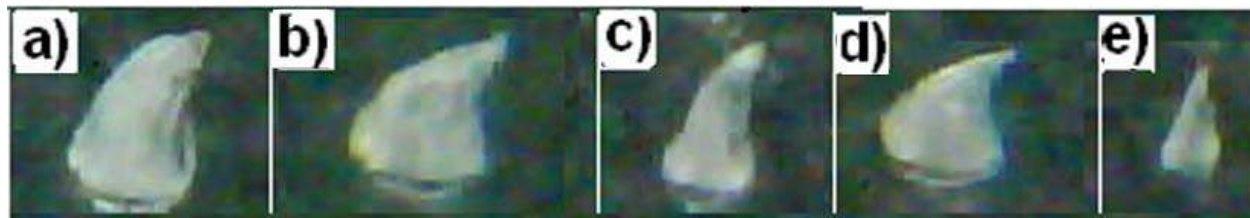


Fig. 5. The ablated bending holes for different scan parameters (Riahi, 2012).

4.2 Ablation of the mixer structure

To fabricate the mixer, a few straight cones and bending cones are ablated with CO₂ laser on two different PMMA sheets. One of the PMMA sheets is CO₂ laser cut to form a channel with two inputs and one output. The structures are then molded with PDMS and one is placed upside down on top of the other. Fig. 6. shows the fabricated channels and holes on the PMMA sheet and the molded PDMS structure.

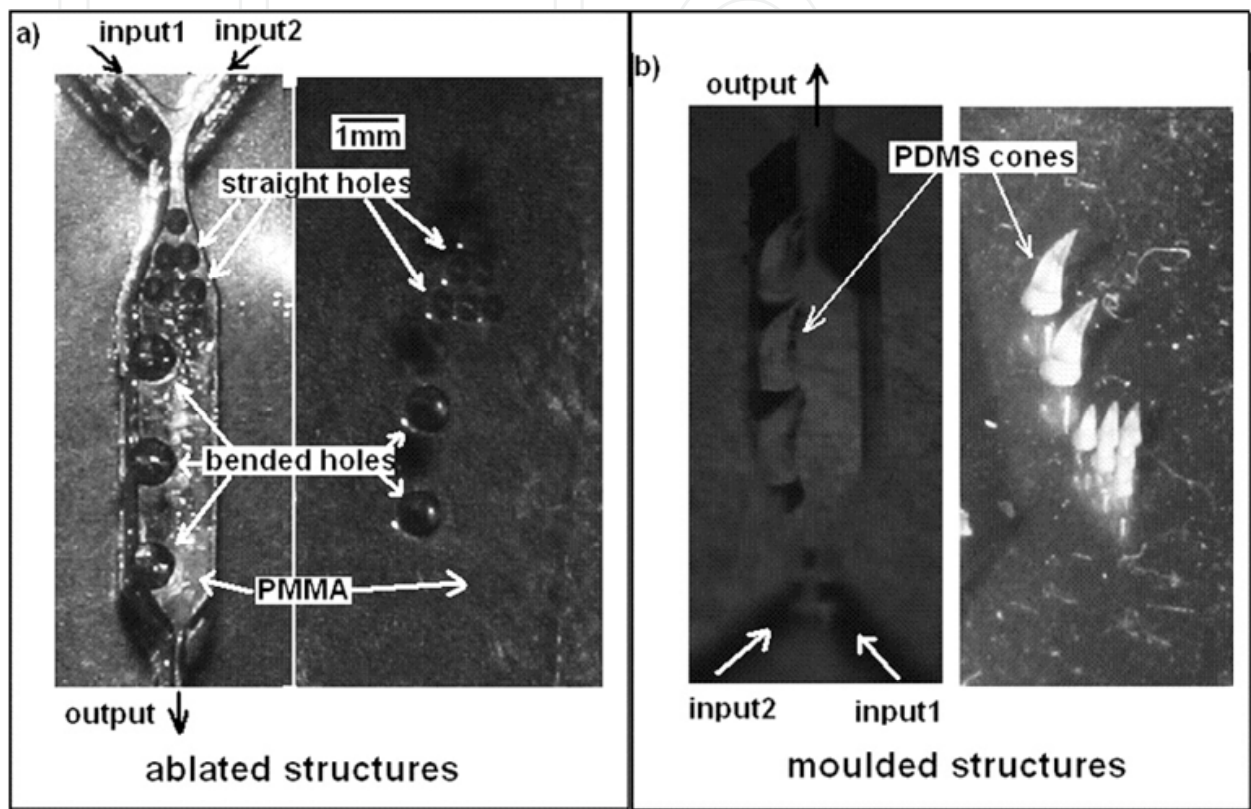


Fig. 6. a) Fabricated structures on PMMA sheets. b) The PDMS molds of structures shown in part a. The straight and bending cones are clear (Riahi, 2012).

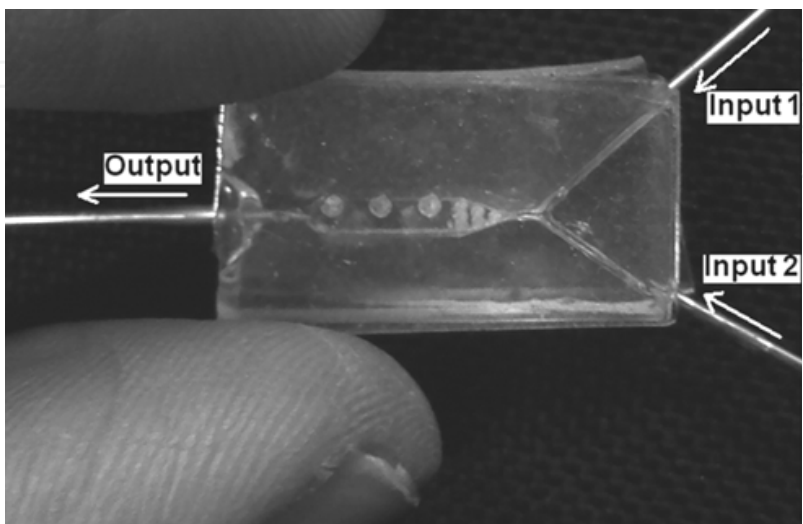


Fig. 7. The fabricated mixer (Riahi, 2012).

The molded PDMS structures are then stacked to each other and three steel tubes are inserted into the input and output channels and the voids are filled with PDMS to form the final mixer structure. The fabricated mixer is shown in Fig. 7.

5. Fabrication of the structures for optofluidics applications

Optofluidics refers to a science that uses the optical property of fluids for adjusting, measuring the properties of a device. Some examples of such devices are, liquid mirrors (Wood, 1909), liquid-crystal displays (Haas, 1983) and liquid lenses (Kuiper & Hendriks, 2004).

Several techniques are used to fabricate a tunable lens array (Dong et al, 2006; Jeong et al, 2004; Xu et al 2009)

In this section we show how a CO2 laser can be used for fabrication of an optofluidic device, liquid micro lens array (Riahi, 2011).

The liquid microlens array is an array of tunable liquid lenses which can be used for Medical stereoendoscopy, Telecommunication, Optical data storage, Photonic imaging, etc.

Fig. 8. shows the basic structure of the liquid lens array which is presented here. An array of the hexagonal holes with about 2mm width each, are first fabricated on a 1mm thick PMMA sheet. A thin layer of PDMS with the thickness of about 50 microns is fabricated and placed on the array of holes. A 1mm depth reservoir with an inlet and outlet for the fluid is also fabricated. The whole of the collection are placed on top of each other.

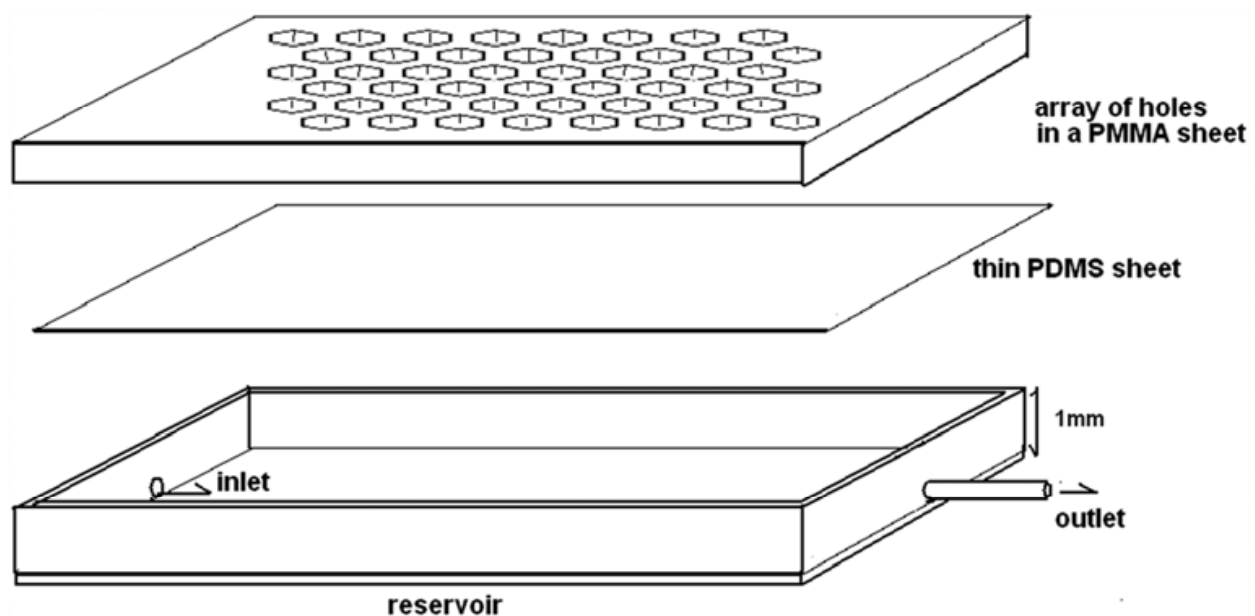


Fig. 8. The structure of a tunable liquid lens array.

By introducing a liquid into the reservoir and changing the pressure inside, the curvature of the PDMS sheet in place of the holes changes and produces convex lenses as shown in Fig. 9.

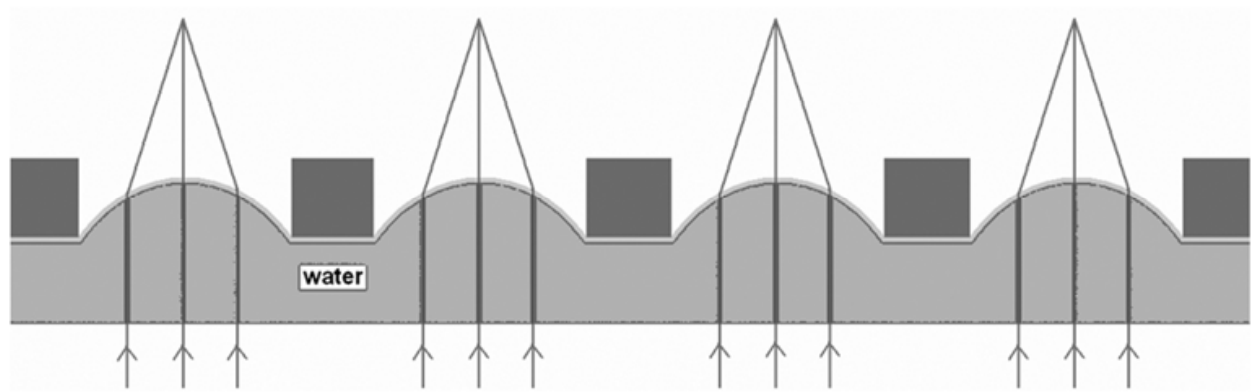


Fig. 9. Mechanism of convex micro lens creation by applying pressure in a water reservoir limited by PDMS and PMMA walls.

As shown in Fig. 10, a commercial CO₂ laser engraving system is used for producing the patterns on PMMA sheets. This engraving machine is also used for fabrication of the reservoir on PMMA sheets.

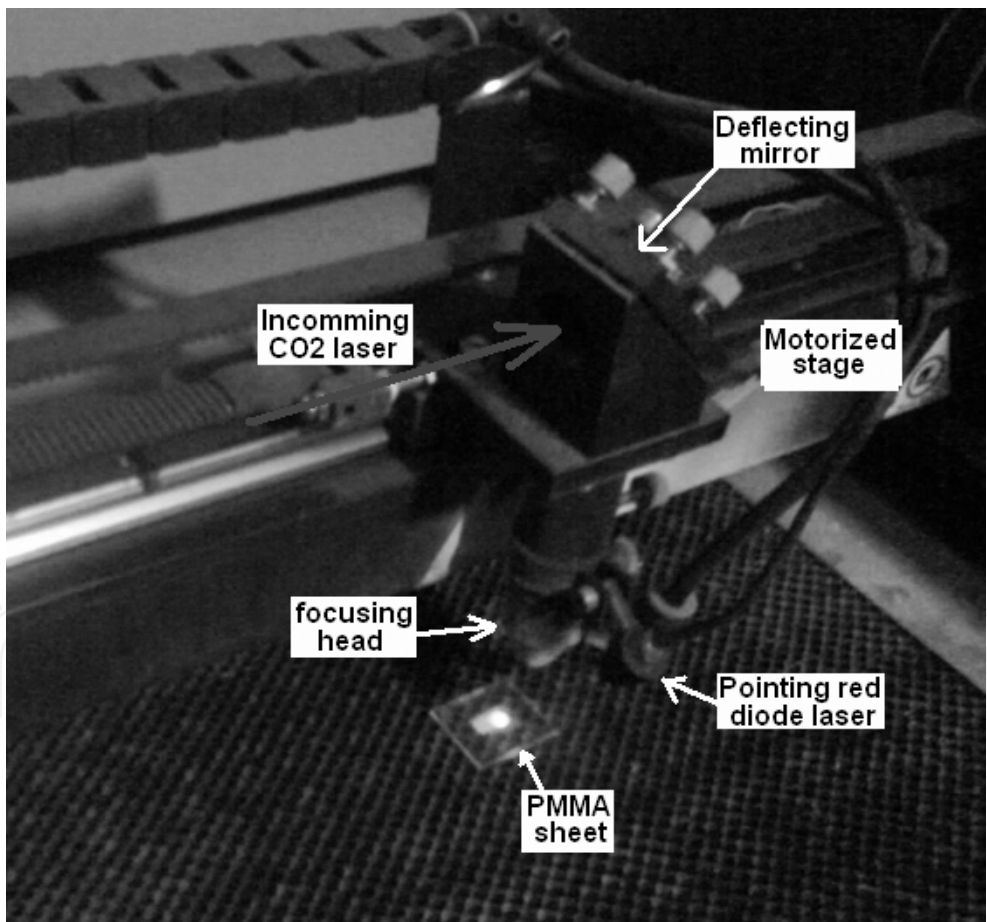


Fig. 10. The commercial CO₂ laser engraving system in production process of an array of hexagonal holes on a PMMA sheet.

Fig. 11 shows the fabricated tunable microlens array with this technique. Fig. 12 also shows this microlens array in imaging from a “B” letter.

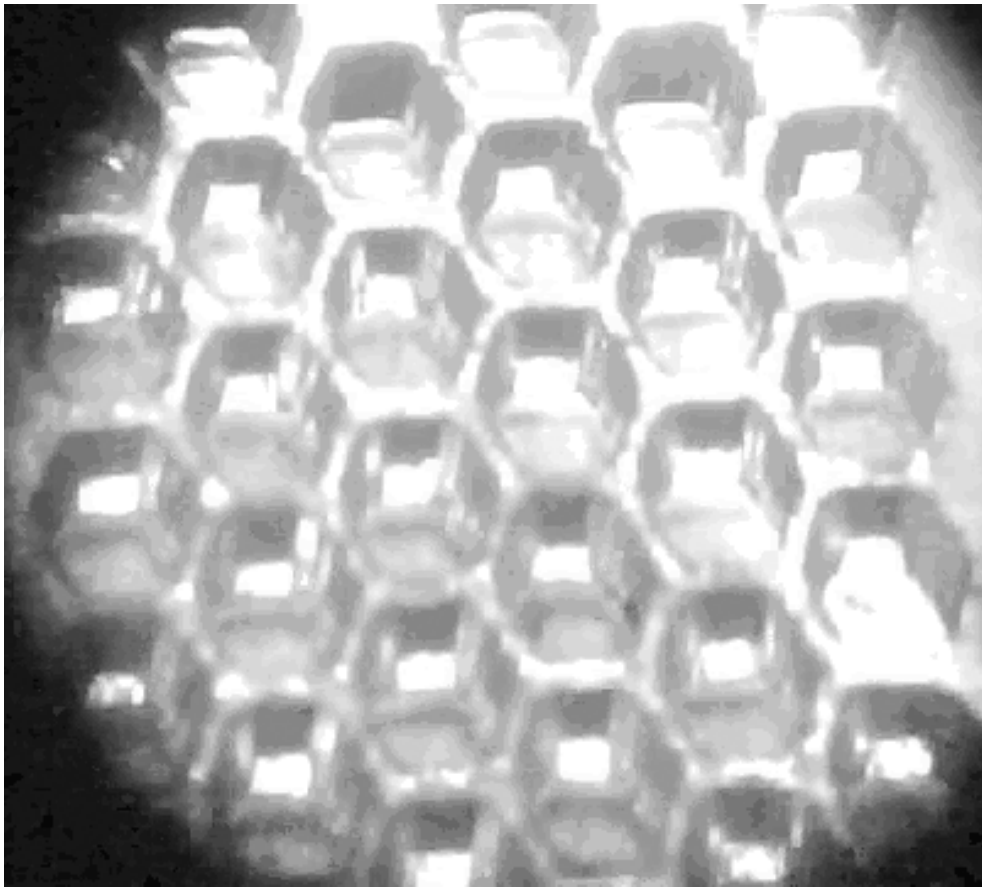


Fig. 11. The fabricated tunable liquid lens array.

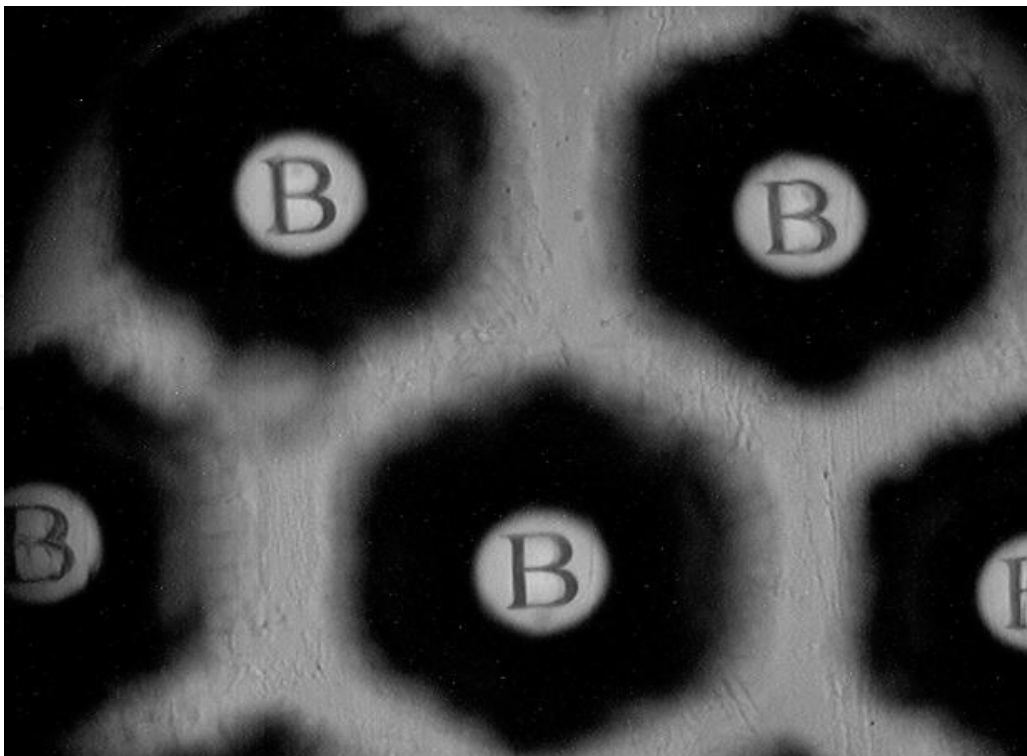


Fig. 12. Imaging from the letter "B" with the fabricated liquid lens array.

6. Fabrication of a beam profiler using the optical properties of liquids

In the previous sections we focused on the application of the CO₂ laser for fabrication of the devices used in microfluidics and optofluidics. In this section we look at the application of a fluid device which is used for CO₂ laser characterization. We present a device called thermally tunable grating (TTG), which can be used as a CO₂ laser beam profiler.

Thermally tunable grating is a family of the gratings which some of their specifications can be adjusted by the user. The tuning ability of a diffractive grating can be divided into two categories: first, gratings in which the diffractive angle can be tuned, and second, gratings in which the intensity of diffraction orders can be modulated which are called grating light valves (GLV). Electrostatic actuation is one of the methods used in MEMS based grating light valves system (Trisnadi et al, 2004). In this grating light valve system, tiny suspended ribbons are put together to form a specular surface. Electrostatic actuation lowers some of the ribbons, and a diffractive grating is formed. Electric field actuation has also been used to actuate an electro-optically controlled liquid crystal based GLV (Chen et al, 1995).

But in TTG device, thermal method is used for actuation of a grating which contains a liquid in its grooves. Increasing temperature, changes the refractive index of the liquid and consequently the diffraction efficiency of the grating (Riahi et al, 2008).

6.1 Principle of the method

As shown in Fig. 13a, we suppose that the grooves of a transparent binary grating with refractive index n_1 are filled with another transparent material with refractive index n_2 . Assume that a laser beam with wavelength λ is incident on this grating. If the period of the grating is large enough compared to the wavelength of light, the rays that pass through the n_1 and n_2 materials will have phases ϕ_1 and ϕ_2 , respectively and the phase difference $\Delta\phi = \phi_1 - \phi_2$ as shown in Fig. 13b.

By changing $\Delta\phi$, the intensity of the diffraction orders is changed as shown in Fig. 13c,d,e. It can be shown that the intensity of the first order of diffraction can be calculated as follow (Riahi et al, 2009):

$$I = I_{\max} \sin^2\left(\frac{\Delta\phi}{2}\right) \quad (2)$$

It is clear now that if n_1 or n_2 are changed, the intensity of the first order of diffraction changes sinusoidally (Fig. 13f).

6.2 Fabrication method

Standard lithography technique is used for fabrication of the binary grating on a glass substrate ($n=1.52$). As shown in Fig 14, the grooves are then filled with nitrobenzene and a thin glass sheet with 250 microns thickness is placed on it. The high boiling point ($T=210.8^\circ\text{C}$), low specific heat capacity (1.51 J/gK), and high dn/dT ($-4.6 \times 10^{-4}\text{ K}^{-1}$ at 626.58 at $T=288\text{ K}$) [36] make nitrobenzene suitable for this work. The refractive index of nitrobenzene is 1.546 at 656.28nm at 293.15 K .

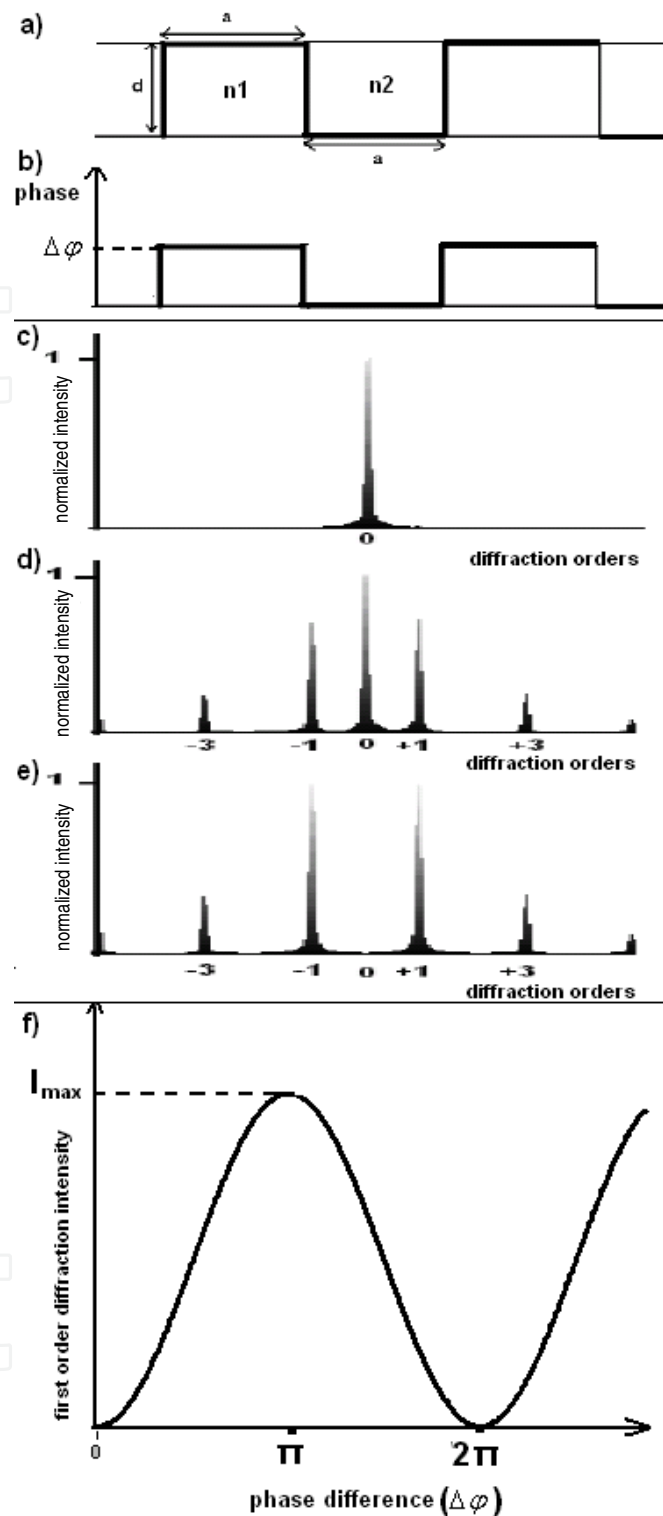


Fig. 13. (a) Square-well grating with n_1 and n_2 for the refractive indices of the land and the groove. (b) Wavefront of an incoming ray immediately after passing through the grating. (c), (d), (e) Simulation results of diffraction from the grating shown in (a) for $\gamma = 0$, $\gamma = \pi/2$, and $\gamma = \pi$, respectively. On the vertical axes, the maximum intensity has been normalized to unity. (f) Results of simulation of the intensity of the 1st order of diffraction versus phase difference (Riahi et al, 2008).

The diffraction pattern and intensity of the first order of diffraction versus temperature has been presented in Fig. 15.

6.3 Measurement of the beam profile of a CO₂ laser

By changing the temperature, the intensity of the 1st order of diffraction is changed. The temperature of the TTG changes upon radiation by a CO₂ laser beam. Radiation of a CO₂ laser beam on a substrate warms it up and produces a temperature profile on the surface of the substrate. The temperature profile depends on the intensity profile of the laser beam. For example, if the laser profile is circular Gaussian, the temperature profile on the surface will be circular Gaussian in ideal case. Now if another visible laser is expanded and diffracted from the surface of the grating, the laser will be diffracted in different amounts from different parts of the grating, containing information on the temperature profile on the grating.

The setup shown in Fig. 16 is used to measure the beam profile of a CO₂ laser. In this setup, a CO₂ laser and a 658nm diode laser are made collinear with each other using a ZnSe window, and finally both lasers are irradiated on a 4mm × 4mm TTG device. The diode laser is expanded to about 3 cm diameter to cover the 4mm × 4mm TTG device with uniform intensity. The CO₂ laser is passed through a shutter so that the irradiation time can be controlled. Immediately after the CO₂ laser pulse, the CCD camera takes a picture from diffracted diode laser by a 4f imaging system using the 1st order of diffraction. It takes about 1 min for the device to get cool enough to repeat the experiment. The heat gun shown in Fig. 16. is used to keep the working area between point A and B as specified in Fig. 15d.

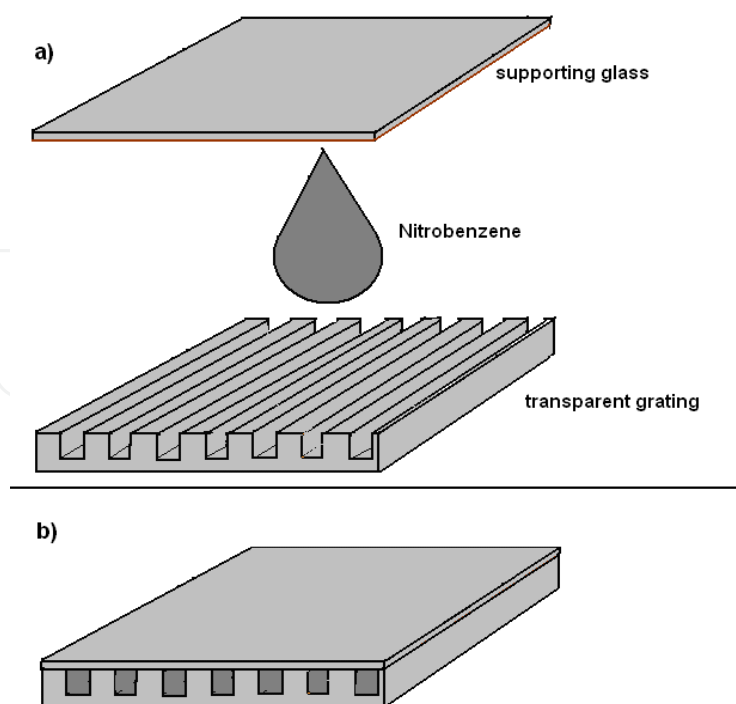


Fig. 14. Fabrication of the TTG device: (a) the grooves of the grating are filled with nitrobenzene and (b) a supporting glass is placed on the device (Riahi et al, 2008).

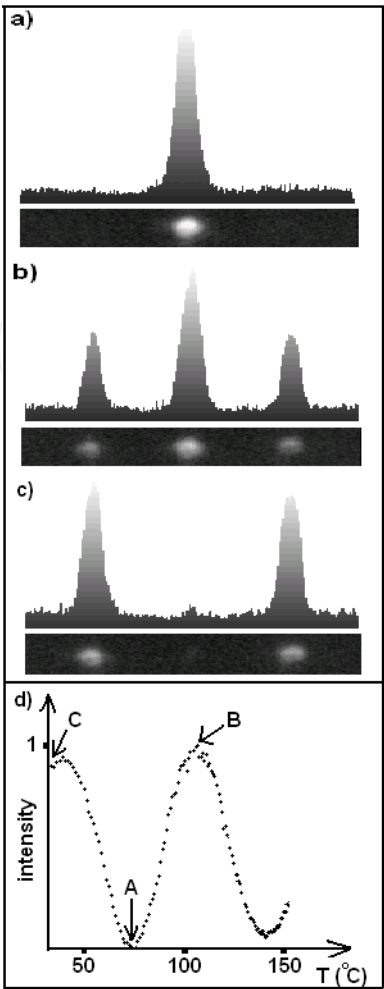


Fig. 15. Diffraction order intensities at different temperatures: (a) $T = 77\text{ }^{\circ}\text{C}$, (b) $T = 108\text{ }^{\circ}\text{C}$, and (c) $T = 140\text{ }^{\circ}\text{C}$. The maximum intensity is normalized to unity. (d) Experimental result of the intensity of the 1st order of diffraction versus temperature. The maximum intensity is normalized to unity (Riahi et al, 2008).

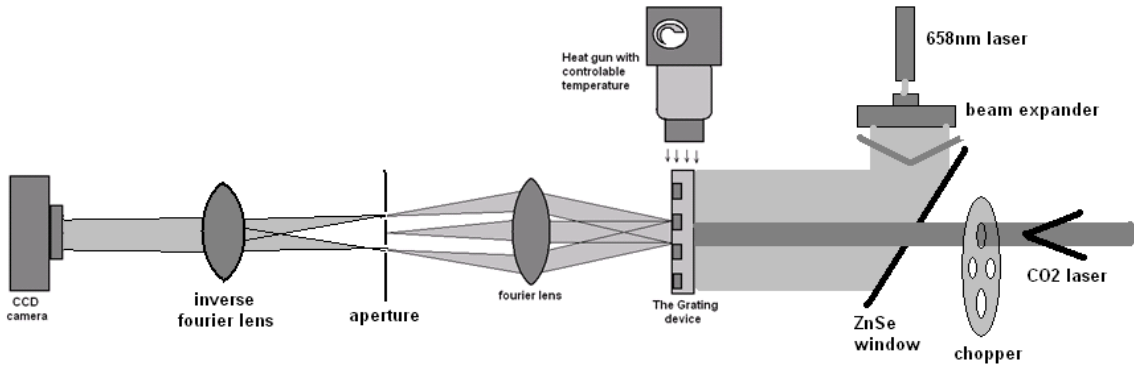


Fig. 16. Setup used for measurement of the temperature profile of the CO2 laser (Riahi et al, 2008).

The Image produced on the CCD camera and measured beam profile of the CO2 laser is shown in Fig. 17.

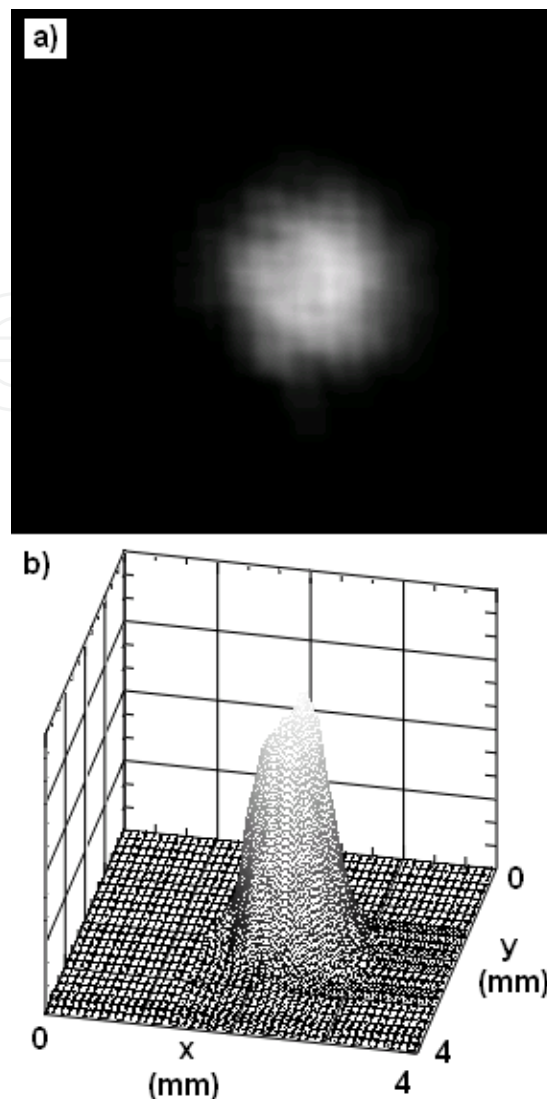


Fig. 17. (a) Image produced on the CCD camera. (b) 3D intensity profile of “a” will be the same as the beam profile of the CO₂ laser (Riahi et al, 2008).

The followings are some errors presented in this experiment.

- additional temperature Gradient on the Thermally Tunable Grating because of the environmental errors
- Thickness of the Supporting Glass
- Aberrations of the Grating
- Expansion of the Grating
- Beam Profile of the Diode Laser

Some of these errors are so small to affect the beam profile, but some of them might be important and have to be corrected.

7. Real time measurement of the CO₂ laser beam profile utilizing TTG

In method we presented in the previous section, after each measurement, time had to be taken for the grating to cool down and get ready for another measurement. This can be a big

problem for real time measurement. In this part, a thermally tunable grating with fast response time is presented, which makes the real time measurements feasible (Riahi & Latifi, 2011).

The principle of this method is the same as what was mentioned in the previous section except that the device becomes a reflective instead of transitive and a thin supporting glass in the device is replaced by a double side polished silicon wafer. The silicon wafer plays the role of a reflector at 532 nm (40% of reflection) and also as an optical window for the CO2 laser. But the most important characteristic of the silicon is its high thermal diffusivity. The thermal diffusivity of silicon is $\alpha_{Si} = 0.95 \text{ (cm}^2/\text{sec)}$. It has to be mentioned that the thermal diffusivity of copper which is used as a very good heat sink is $\alpha_{Cu} = 1.1 \text{ (cm}^2/\text{sec)}$ which is just a bit more than for silicon.

However, silicon can play a role of a heat sink during the measurements and make the real time measurements feasible.

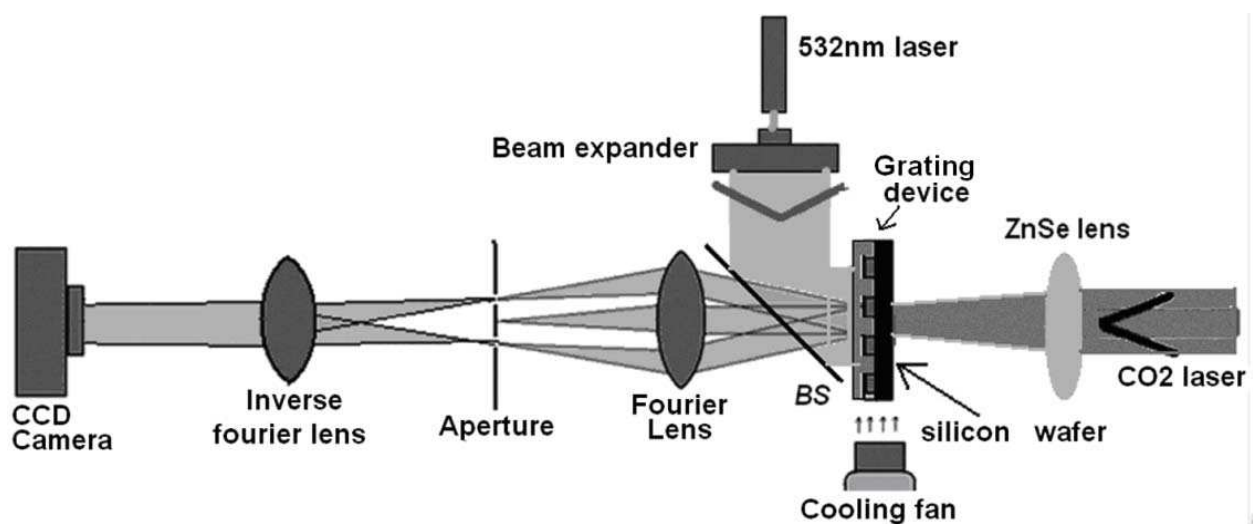


Fig. 18. Schematic setup for real time measurement of the CO2 laser beam profile (Riahi & Latifi, 2011)

To measure the beam profile of a CO2 laser, a setup as shown in Fig. 18 was used. In this setup, a CO2 laser beam incident on the grating device from the silicon side is absorbed in the grating structure and warms it up. A 532 nm laser is expanded and irradiates the grating, from the glass side. After passing through the grating, the visible light reflects back from the silicon slab and is directed to a 4f imaging system. A high pass spatial filter is used to keep the first order of diffraction for imaging.

The response time of this system can be measured. For this reason the same setup as in Fig. 18 is used, except that a chopper is placed in front of the CO2 laser and a fast photo-detector is used instead of the CCD camera. By chopping the CO2 laser beam, the signal of the photo-detector was monitored by an oscilloscope. As seen in Fig. 19, the response time of this device is about 10 milliseconds.

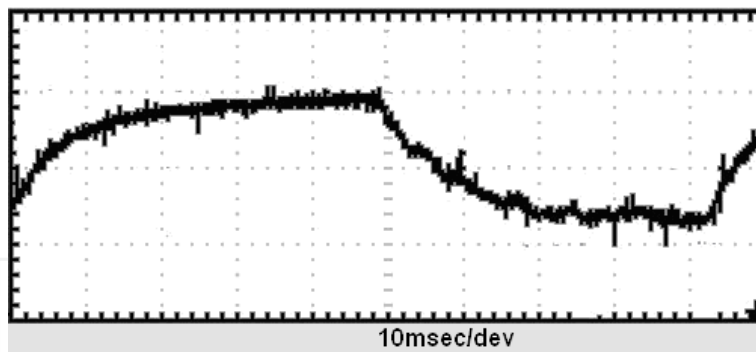


Fig. 19. Detected signals from photo-diode when CO₂ laser is chopped off and on

8. Conclusion

In this chapter, the relation between CO₂ laser and fluid applications was presented. First, application of a CO₂ laser for fabrication of microfluidic and optofluidic structures on PMMA polymer was presented. Then application of a fluidic device for measurement of a characteristic of a CO₂ laser was discussed.

Application of the CO₂ laser for microfluidic fabrication is a simple and low cost method which can be performed by a commercial CO₂ laser engraving system. This method makes the final products very cheap which are suitable for single use applications.

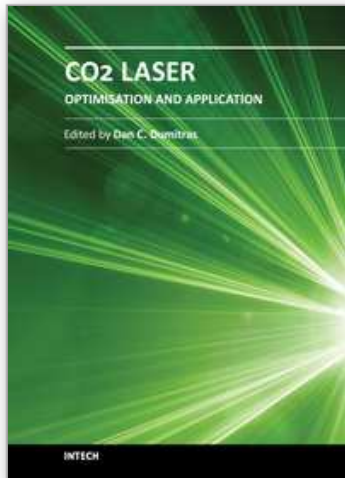
Also it seems that the application of the CO₂ laser in microfluidics shows a good potential for fabrication of some complicated structures even 3D structures for future works.

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The present book includes several contributions aiming a deeper understanding of the basic processes in the operation of CO₂ lasers (lasing on non-traditional bands, frequency stabilization, photoacoustic spectroscopy) and achievement of new systems (CO₂ lasers generating ultrashort pulses or high average power, lasers based on diffusion cooled V-fold geometry, transmission of IR radiation through hollow core microstructured fibers). The second part of the book is dedicated to applications in material processing (heat treatment, welding, synthesis of new materials, micro fluidics) and in medicine (clinical applications, dentistry, non-ablative therapy, acceleration of protons for cancer treatment).

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