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## Three-Dimensional Printing: A Novel Technology for Use in Oral and Maxillofacial Operations

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Additional information is available at the end of the chapter

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#### **Abstract**

Three-dimensional (3D) printing is cited as "a novel, fascinating, future builder technology" in many papers and articles. Use of this technology in the field of medicine and especially oral and maxillofacial surgery is expanding. The type of manufacturing systems, materials, cost-effectiveness, and also bio-printing, with studies from around the world today, make this field a "hot-topic" in reconstructive and regenerative surgery. This chapter evaluates the latest updates and scientific uses of 3D printing.

**Keywords:** Rapid prototyping, three-dimensional printing, reconstructive surgery, oral, maxillofacial surgery

#### 1. Introduction

Three-dimensional printing (3D), also known as rapid prototyping (RP), was first introduced in the 1980s. During the past three decades, enormous changes and developments have been made by scientists modifying this technology, materials, and accuracy. Within the field of craniofacial surgery, 3D surgical models have been used as templates to harvest bone grafts, tailoring bioprosthetic implants, plate bending, cutting guides for osteotomies, and intraoperative oral splints. Using 3D models and guides has been shown to shorten the operative time and reduce the complications associated with it. The ultimate goal of any surgical procedure is to improve peri-operative form and function and to minimize operative and postoperative morbidity. Many exciting and new technological advances have opened a new



era in the field of oral and maxillofacial surgery over the last years, and 3D printing is among the most novel. The aim of this chapter is to introduce 3D printing method and its role in contemporary oral and maxillofacial surgery and to review different applications and benefits of 3D printing-assisted surgeries in the oral and maxillofacial region.

#### 2. History and benefits

Three-dimensional printing has been utilized in diverse aspects of manufacturing to produce different objects from guns, boats, and food to models of unborn babies. From over 1450 articles related to 3D printing listed in PubMed, nearly a third of them were published in the last 2 years [1].

3D printing is a manufacturing process wherein objects are fabricated in a layering method during fusing or depositing different materials such as plastic, metal, ceramics, powders, liquids, or even living cells to build a 3D structure [2, 3]. It is a process of generating physical models from digital layouts [4, 5]. This technology demonstrates a technique where a product designed via a computer-aided scheme is manufactured in a layer-by-layer system [6]. This process is also known as RP, solid freeform technology (SFF), or additive manufacturing (AM) [7].

3D printing techniques are not new and have existed since 30 years ago [8–10]. This technology was first introduced and invented by Charles Hull in 1986, and at first it was utilized in the engineering and automobile industry for manufacturing polyurethane frameworks for different models, pieces, and instruments [11]. Originally, Hull employed the phrase "Stereo-lithography" in his US Patent 4,575,330, termed "Apparatus for Production of Three – Dimensional Objects by Stereolithography" published in 1986. Stereolithography (SL) technique included subjoining layers over the top of each other, by curing photopolymers with UV lasers [12, 13].

Since then, 3D models have been used for a diversity of different objectives. Since 1986, this process has started to accelerate and has honored recognition globally and has influenced different arenas, such as medicine. The developing agora for 3D desktop printers encourages wide-ranging experimentations in all fields. Generally, medical indications of these printers are treatment planning, prosthesis implant fabrications, medical training, and other usages [4]. Having being used in the military, food industry, and arts, RP has received much attention in the field of surgery in the last 10 years [6, 14]. The pioneering usage of SL in oral and maxillofacial surgery was by Brix and Lambrecht in 1985. Later, this technique was used by them for treatment planning in craniofacial surgery [15]. In 1990, SL was used by Mankovich et al. for treating patients having craniofacial deformities [16, 17]. They used it to simulate bony anatomy of the cranium using computed tomography (CT) with complete internal components [17, 18].

By aiding in complex craniofacial reconstructions, 3D printing has recently earned reputation in medicine and surgical fields [19–21]. Today, maxillofacial surgery can benefit from additive

manufacturing in various aspects and different clinical cases [22]. This technique can help with bending plates, manufacturing templates for bone grafts, tailoring implants, osteotomy guides, and intraoperative occlusal splints [23–27]. RP can shorten surgery duration and simplify preand intraoperative decisions. It has enhanced efficacy and preciseness of surgeries (**Table 1**) [10].

Diagnosis and treatment planning

Direct visualization of anatomic structures

Surgical guides/templates

Surgical practice/rehearsal

Designing incisions

Surgical resections

Assessment of bony defects for grafting

Adaptation/pre-bending of reconstruction plates

Fabrication of custom prostheses

TMJ prostheses, distraction devices, fixation devices

Decreased surgical time, anesthesia time, wound exposure duration

More predictable results

Improved colleague communication

Educational tool for patients

Table 1. Uses of 3D models [22].

#### 3. Manufacturing process and types of models

There are different technologies introduced for 3D printing. Binder jetting (BJ), electron beam melting (EBM), fused deposition modeling (FDM), indirect processes, laser melting (LM), laser sintering (LS), material jetting (MJ), photopolymer jetting (PJ), and SL are well-known technologies of 3D printing [14, 28, 29]. There are many different 3D printing techniques. Benefits and disadvantages are factors inherent to each technology system [14]. Among this variety of different techniques, there is a huge demand for oral and maxillofacial surgery for SL, FDM, and PJ [1, 28, 30]. **Table 2** summarizes some different three-dimensional printing technologies.

#### 3.1. Stereolithography (SL)

The initial 3D printing technique SL began in the late 1980s [31]. The original SL uses a laser beam for resin polymerization in two-dimensional patterns [32]. Being the pioneering additive manufacturing method, SL produces 3D objects by curing layers of liquid photopolymer or

epoxy resin with a low-power UV laser [13]. SL projects a UV laser to a cross section of a single layer of the resin onto a photopolymer resulting in the setting of the layer. This is repeated until fabricating all zones of the product [1]. This technique utilizes a mirror to guide the laser to the surface in a layer-by-layer manner. Furthermore, the 3D device projects it on the surface resins. This procedure is done from the base to the surface (Figure 1) [14, 33].

| Techniques  | Advantages   | Disadvantages   |
|---|--|---|
|   | Light cured resin  |   |
| 1. Stereolithography (SL) —Light-sensitive polymer cured layer by layer by a scanning laser in a vat of liquid polymer  |  | Only available with light curable liquid polymers. Support materials must be removed. Resin is messy and can cause skin sensitization and may be irritant by contact and inhalation. Limited shelf life and vat life. Cannot be heat sterilized. High-cost technology                     |
| 2. Photojet—Light-sensitive polymer is jetted onto a build platform from an inkjet-type print head and cured layer by layer on an incrementally descending platform                         | Relatively fast. High-resolution,<br>high-quality finish possible.<br>Multiple materials are available<br>with various colors and physical<br>properties including elastic<br>materials. Lower cost technology | Tenacious support material can be difficult to remove completely. Support material may cause skin irritation.  Cannot be heat sterilized. High- cost materials  |
| 3. DLP (digital light processing)—Liquid resin is cured layer by layer by a projector light source.  The object is built upside down on an incrementally elevating platform                 | Good accuracy, smooth surfaces, relatively fast. Lower cost technology   | Light curable liquid polymers and wax-<br>like materials for casting. Support<br>materials must be removed. Resins are<br>messy, can cause skin sensitization, and<br>may be irritant by contact. Limited shelf<br>life and vat life. Cannot be heat<br>sterilized. Higher cost materials |
|   | Powder binder  |   |
| Plaster or cementaceous material set by<br>drops of (colored) water from<br>"inkjet" print head. Object built layer by<br>layer in a powder bed, on an incrementally<br>descending platform | Lower cost materials and<br>technology. Can print in color.<br>Unset material<br>provides support. Relatively fast<br>process. Safe materials  | Low resolution. Messy powder. Low strength. Cannot be soaked or heat sterilized   |
|   | Sintered powder  |   |
| —Object built layer by layer in powder bed. Heated build chamber raises temperature of material to just below melting point.  | Range of polymeric materials including nylon, elastomers, and composites. Strong and accurate parts. Self-supported process. Polymeric   | Significant infrastructure required, e.g., compressed air, climate control. Messy powders. Lower cost in bulk. Inhalation risk. High-cost technology. Rough surface   |
| Scanning laser then sinters powder  | materials—commonly nylon may   | 7   |

layer by layer in a descending bed be autoclaved. Printed object may

| Techniques  | Advantages   | Disadvantages   |
|---|--|---|
|   | have full mechanical functionality.  Lower cost materials if used in large volume  |   |
| Selective laser sintering (SLS) —for metals and metal alloys. Also described as selective laser melting (SLM) or direct metal laser sintering (DMLS). Scanning laser sinters metal powder layer by layer in a cold build chamber as the build platform descends. Support structure used to tether objects to build platform | steel. Metal alloy may be  | Elaborate infrastructure requirements. Extremely costly technology. Moderately costly materials. Dust and nanoparticle condensate may be hazardous to health. Explosive risk. Rough surface. Elaborate post-processing is required: Heat treatment to relieve internal stresses in printed objects. Hard to remove support materials. Relatively slow process |
| Electron beam melting (EBM, Arcam).  Heated build chamber. Powder sintered layer by layer by scanning electron beam on descending build platform  | High-temperature process, so no support or heat treatment needed afterward. High speed. Dense parts with controlled porosity  Thermoplastic                            | Extremely costly technology moderately costly materials. Dust may be hazardous to health. Explosive risk. Rough surface. Less post -processing required. Lower resolution   |
| Fused deposition modeling (FDM) First 3DP technology, most used in "home" printers. Thermoplastic material extruded through nozzle onto build platform  | High porosity. Variable mechanical strength. Low-to-mid-range cost materials and equipment . Low accuracy in low-cost equipment. Some materials may be heat sterilized | Low cost but limited materials— only thermoplastics. Limited shape complexity for biological materials. Support material must be removed  |

Table 2. 3D printing modalities and materials [14].

It is necessary to extract waste materials manually from the eventual outcome [34-36]. Nowadays, SL is known as the gold standard in 3D manufacturing with yield resolutions up to 0.025 mm. SL is reliable in reconstruction of internal frameworks and is more efficient in fabricating larger objects [37]. SL is largely accepted to have the best surfacing and the most accuracy of any 3D technology. Materials used in this system must be to some degree brittle and light [38, 39]. Acrylics and epoxies are commonly used for this method [40]. However, SL still requires manual handling after fabrication, and the process lasts more than a day to be completed. SL is more expensive than other techniques due to materials used, and the printer is considered more expensive due to the high cost of the raw materials and device maintenance [23, 41]. SL is largely utilized for producing implant drill guides [14]. The ability to build complex and detailed structures, extraction of waste resin without difficulty, and extremely high resolution (~1.2 um) are considered main advantages of SL [42] feature.

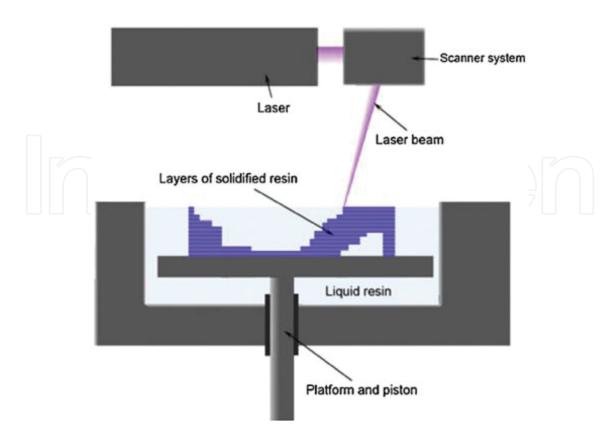


Figure 1. Schematic view of SL [115].

#### 3.2. Fused deposition modeling

FDM uses a similar principle to SL in that it builds models on a layer-by-layer basis. When there is a discussion about cost-effectiveness, FDM is considered among the most utilized consumer 3D printing methods [16, 43, 44]. In FDM, a melted filament of thermoplastic material is extruded from a nozzle moving in the x-y plane and solidifies upon deposition on a build plate [45]. The build plate is lowered by 0.1 mm after each layer reappears. The process is repeated until the final product is produced. The most frequently used raw materials in FDM printers are acrylonitrile-butadiene-styrene (ABS) and polylactic acid (PLA) materials known for being key components of scaffold structures used for "bioprinting" [40].

Notable disadvantage and shortcoming for FDM is disability to form complex structures and most anatomical structures with complex shapes. For manufacturing a clean product, hollow internal structures or blind-ended openings are especially troublesome. Almost all household FDM printers are currently limited in mono-color and mono-material for manufacturing. However, this can be overcome by recently developed dual-extruder technology. In this technology, two filaments of different colors or materials can be extruded from a common printer head. MakerBot Replicator 2X Experimental (MakerBot Industries, New York, NY, USA), Cube 3 (3D Systems, Rock Hill, SC, USA), and Creatr x1 (Leapfrog, Emeryville, CA, USA) are known for this ability. Even more, the second extruder can be configured to build

support structures using MakerBot Dissolvable Filament (MakerBot Industries), made of high-impact polystyrene (HIPS) [6, 46].

Support structures are required for FDM models such as SL as thermoplastic needs time to harden and also the layers to bond together [47]. Since multiple extrusion nozzles can be used in FDM, each with a different material, there is no theoretical restriction on compositional gradients in all three dimensions for FDM. High porosity due to the laydown pattern and good mechanical strength are notable and key advantages of FDM (**Figure 2**).

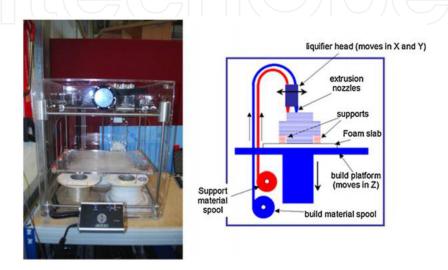


Figure 2. Schematic view of FDM [40].

#### 3.3. PolyJet modeling

Multijet modeling printing, also known as MultiJet Printing (3D Systems, Rock Hill, SC, USA) or PolyJet Technology (Stratasys, Edina, MN, USA), is similar to SL; the difference is that the liquid photopolymer is immediately cured by UV light [48]. Multijet modeling printing can manufacture prototypes with high resolution (16  $\mu$ ) that is comparable to or even better than SL. The advantage is the capacity to print in multiple materials for the desired degree of tensile strength and durability. An MJM printer is easier to maintain than an SL system. On the contrary, a disadvantage is the high price of these printers which makes MJM( Multi Jet Modeling) more suitable for large-scale productions rather than for office-based applications (**Figure 3**) [6].

The drawback is that the equipment and materials are costly to purchase and run, and the support materials can be tenacious and rather unpleasant to remove. They are useful for printing dental or anatomical study models, but these are expensive when produced. A particular advantage of this technology is that the use of multiple print heads allows simultaneous printing with different materials, and graduated mixtures of materials, makes it possible to vary the properties of the printed object, which may for example have flexible and rigid parts, for the production of indirect orthodontic bracket splints [14].

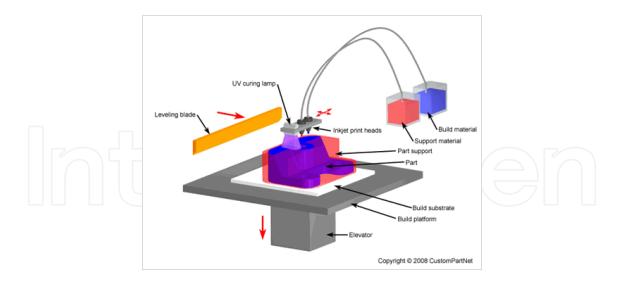


Figure 3. Schematic view of PolyJet [116].

#### 4. Accuracy of 3D printing

Additive manufacturing plays a critical role in craniomaxillofacial surgery [49].

3D models simulate anatomy of the human body and can be extensively useful in oral and maxillofacial surgery. These models are of great value in decision making [50]. 3D models must be precise and extremely accurate in simulating head and neck anatomy to be beneficial in maxillofacial surgery. Faulty and inexact models can jeopardize diagnosis and treatment planning [16, 51]. There is limited data available about evaluation of the accuracy of 3D printed models. Inaccurate models can cause dramatic errors in treatment planning and simulations [49]. 3D printer accuracy generally depends on the accuracy of CT scans. CT is modality of choice for 3D printing purposes. While obtaining CT images, each slice thickness must be as thin as possible (1-2 mm) [30]. At present, no gold standard is introduced for measuring the accuracy of medical 3D models [49]. The accuracy of different additive manufacturing technologies is examined by researchers in maxillofacial surgery globally. The literature indicates that different techniques have different accuracy levels in reconstructing maxillofacial structures using 3D printing. As mentioned before, experiences have pointed out that SL creates 3D models with great accuracy. Average deviation of SL models varies from 0.20–0.85 mm. Error percentage in these models is between 0.6 and 6% [17, 30, 52-54]. Peter Shih-Hsin Chang et al. investigated the accuracy of SL for modeling midface irregularities. This was done comparing distances between key landmarks on the skulls and 3D models. Average overall difference between replicas and cadaver samples was between 0.8 and 2.5 mm in all locations. They stated that SL preciseness is affected by variants in different stages of manufacturing such as data collection and transfer, product fabrication, and maintenance [38]. Preciseness and accuracy is critical in orthognathic surgery for gaining better results both esthetically and functionally. In a recent study, Shqaidef et al. evaluated the accuracy of 3D printed wafers of 10 orthognathic patients. After aligning with dental models, the absolute mean error of the wafers was 0.94 (0.09) mm. In this research, they showed error in 3D printed models is up to 1.73 mm which is considerable and will distort skeletal movements [55]. In another study, the PolyJet technique had the most precise fabrication in simulating mandibular architecture [50].

Salmi et al. assessed the accuracy of different 3D printing techniques by measuring balls attached to each 3D model. It was concluded that the PolyJet technique had the least inaccuracies [49].

Table 3 demonstrates results of different studies with accuracy measurement of 3D printed

| Authors   | Comparisons                          | Mean difference (%)  | Measuring equipment                  |
|---|--------------------------------------|----------------------|--------------------------------------|
| Salmi et al. (2013)                               | SLS e 3D CT (original 1. & 2. model) | 0.79 0.26 & 0.80     | Coordinate measuring machine         |
|   | 3DP e 3D CT (original 1. & 2.        | 0.320.67 0.43 & 0.69 | and measuring balls & Pro            |
|   | measurement) 3DP e 3D CT (moderate)  | 0.440.38 0.220.55    | Engineer software for 3D models      |
|   | 3DP e 3D CT (worse)PolyJet e 3D CT   | 0.370.18 0.12 & 0.18 |                                      |
|   | (original 1. & 2. measurement)       | 0.13                 |                                      |
| El-Katatny et al.                                 | FDM e 3D CT                          | 0.24 0.160.22 0.11   | Digital caliper                      |
| (2010)  | skullFDM e 3D CT mandible            |                      |                                      |
| Ibrahim et al. (2009)                             | SLS e dry mandible3DP e dry          | 1.793.142.14         | Digital caliper and test indicator   |
|   | mandiblePolyJet e dry mandible       |                      | attached to electric milling machine |
| Silva et al. (2008)                               | SLS e dry skull3DP e dry skull       | 2.102.67             | Digital caliper                      |
| Nizam et al.(2006)                                | SL e dry skull                       | 0.08 1.25            | Digital caliper                      |
| Chang et al. (2003)                               | 3DP e fresh skull                    | 2.1e4.7              | Dial caliper                         |
| Choi et al. (2002) SL e dry skullSL e 3D CT skull |                                      | 0.56 0.390.82 0.52   | Caliper & MagicsviewSoftware         |
|   |                                      |                      | for 3D model                         |
| Asaumi et al. (2001)                              | 3D CT e dry skullSL e dry skull      | 2.160.63             | Caliper & 3DCT images                |
| Berry et al. (1997)                               | SLS e 3D CT                          | 0.64                 | None reported                        |
| Barker et al. (1994)                              | SL e dry skull                       | 0.6e3.6              |                                      |
| Ono et al. (1994)                                 | SL e dry skull                       | 3                    |                                      |
| Waitzman et al. (1992)                            | 3D CT e dry skull                    | 0.9 (0.1e3.0)        | CT images & caliper                  |

Dawood, A., B. M. Marti, V. Sauret-Jackson and A. Darwood (2015). "3D printing in dentistry." British dental journal **219**(11): 521-529.

Mehra, P., J. Miner, R. D'Innocenzo and M. Nadershah (2011). "Use of 3-d stereolithographic models in oral and maxillofacial surgery." *Journal of maxillofacial and oral surgery* **10**(1): 6-13.

Salmi, M., K.-S. Paloheimo, J. Tuomi, J. Wolff and A. Mäkitie (2013). "Accuracy of medical models made by additive manufacturing (rapid manufacturing)." Journal of Cranio-Maxillofacial Surgery 41(7): 603-609.

Table 3. Studies with accuracy measurement of AM models [49].

#### 5. Clinical applications

Three-dimensional printing has been available for over three decades. Despite that, medicine has benefitted from its application recently [23–25]. As mentioned before, 3D printed models can be useful in different aspects of maxillofacial surgery such as templates, splints, tailored implants, and others [23–27]. These models can reduce surgery duration and enhance the results [10]. RP technology can become very useful for both doctor and patients in treatment planning for each patient individually [56]. Medical applications of 3D printers have expanded after recent advancements of these systems. In oral and maxillofacial surgery, 3D printing methods have been utilized for different purposes including distraction osteogenesis and treatment of craniofacial deformities [57, 58]. The following are the main applications of 3D printing technology in oral and maxillofacial surgery:

#### 5.1. Surgical planning

Since 3D printing can distinguish traumatic and pathologic defects more effectively, it has proven to enhance diagnosis and treatment in the maxillofacial region. This feature results in precise decision making. In the aspect of pathologic lesions, 3D printing is capable of presenting spatial relationships to surrounding components [52–54, 58–63]. These important visualizations can minimize operative complications [26].

By 3D printing, surgeons can visualize the procedure and forecast the challenges to gain better results before they even start. Three-dimensional printing can produce models rapidly with acceptable accuracy and structural details to allow for better outcomes and reduced operating durations [64].

#### 5.2. Trauma surgery

3D printers can facilitate the treatment of trauma patients with recent or delayed fractures and defects. Different fractures of maxillofacial structures can benefit from 3D printing but orbital wall fractures are the best targets for these methods [65–67]. These patients can be treated by 3D customized reconstruction of orbital wall defects with titanium mesh or sheet [68]. Before the surgery begins, titanium mesh or plate is adapted precisely on the 3D printed replica to help shortening the duration of general anesthesia [69, 70].

Complicated and detailed anatomy of the orbit makes it difficult to reconstruct orbital defects. Postoperative enophthalmos or diplopia always happens without accurate and proper reconstruction of orbital walls. Surgeons can solve these complications by using 3D printed titanium mesh using the contralateral orbital anatomy [30, 71].

Sas a et al. evaluated the application of custom-made implants using 3D printing system to reconstruct in blowout fractures of the orbital floor. After the surgery, average orbital volume (OV) of the affected side noticeably decreased, and OV of corrected orbit was not different compared to the unaffected side [72].

Chandan Jadhav et al. treated three patients with medial orbital wall fractures using 3D models. They used the 3D model as a template to measure and harvest bone graft from iliac

crest easily and precisely, resulting in perfect adaptation and reduced operation time (Figures 4 and 5) [56].



Figure 4. The rapid prototype metal orbital floor reconstruction in the orbit of the stereolithic skull reconstructed from the original CT scans [71].

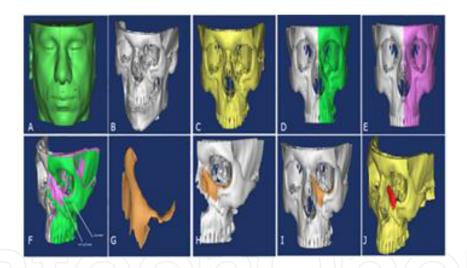


Figure 5. Treatment of orbital floor defect in a trauma patient using 3D printing technology. (a) 3D model designed based on CT scan images; (b) removal of soft tissue on differences between soft and hard tissue density; (c) removal of excess bone; (d) dividing the face into two halves from symmetry line; (e) mirroring the uninjured side on the other side; (f) comparison of the injured half and the mirrored half and finding their differences; (g) differentiation of the ideal design; (h) precise adaption on injured half; (i) correction of the design by removal of excess components; (j) final model.

#### 5.3. Orthognathic surgery

Precise planning and decision making based on exact diagnosis is critical in the success of orthognathic surgeries [73]. As mentioned earlier, 3D printing technology shows some clinically noticeable inaccuracies for orthognathic surgery which is troublesome for ideal dental occlusion [30].

#### 5.4. Facial prosthetics

There are reports of fabricating prosthetic nose [74, 75], ears [76, 77], eyes [78, 79], and face [80, 81], in the last 10 years. Literature indicates that better esthetic and functional outcomes are accomplished with the application of 3D printing in comparison to the traditional prosthetics (Figure 6) [76, 82].

Facial prosthetics fabricated with RP methods are being utilized successfully. Ancient Egyptians were the first people to apply facial prosthetics in 500 B.C [83].

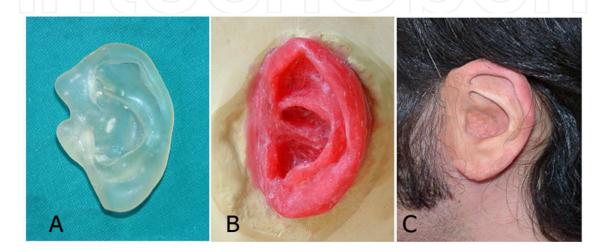


Figure 6. (a) 3D model obtained by stereolithography; (b) stereolithographic model turned into wax; (c) finished auricular prosthesis [85].



Figure 7. Application of 3D printing in lateral nasal osteotomy. (a) Planned osteotomy lines of lateral nasal osteotomy are drawn with a skin marker on the 3D model; (b) compensate the thickness of the soft tissue lining of the nose with thick wax; (c) trimming the custom-made splint on the 3D model; (d) performing the lateral nasal osteotomy in line with the surgical plan; (e) pre- and postoperative views [117].

Facial prosthetics have evolved extensively with the application of 3D printing technology. This technique allows producing replicas of facial structure within just hours [84].

Impression procedures are the common method to manufacture facial prosthetics. Longer duration of production, soft tissue distortion, and patient discomfort are the main limitations of this process. Lately, 3D printing has been utilized to produce facial prosthetics to reduce limitations of traditional procedures. Additive manufacturing technology can simplify the procedure, shorten laboratory procedures by excluding impression procedures, and model wax-ups. No doubt, 3D printing will become the modality of choice to manufacture facial prosthetics [85]. Additive manufacturing is mainly used for hard tissue reconstruction. However, it is useful in soft tissue contouring [5, 86] such as auricular reconstruction in patients using the contralateral ear (**Figure 7**) [87].

Auricular prosthesis production consists of multiple time-consuming processes demanding patient presence. These procedures are (1) impression making, (2) fabricating a wax replica, (3) manufacturing a mold, and (4) creating the prosthetic object with a suitable color. 3D printing technique simplifies and shrinks the first three steps. The process can be completed in 24–48 hours instead of a week [88].

#### 5.5. Customized TMJ reconstruction

In the field of TMJ(Temporomandibular Joint) reconstruction, sufficient exposure and access is critical to prevent damaging many vital structures in this area. Alloplasts and allografts must be accurately placed to regain correct function of the jaw [89]. 3D printing can become useful in the treatment of TMD(Temporomandibular Joint Disorders) patients with total condylar resorption [18]. Mehra et al. treated a patient by bone grafting and TMJ prostheses using additive manufacturing. 3D printing aided in measuring exact proportions of the bone needs to be harvested [22].

#### 5.6. Dental implants

Creation of new dental implants has benefitted from 3D printing technology [90, 91].

3D printing acts as a tool to create dental implants with complicated geometries [14].

Drilling guides are of great value to transfer implants from their planned positions. Manufacturing a drilling guide by conventional methods is time-consuming and requires multiple patient visits and extensive laboratory work. RP facilitates this with solely a single consultation prior to operation. In this session, data are gathered, and the guide is virtually built and later will be manufactured by the 3D device [92].

#### 5.7. Complex facial reconstruction

Pathologic lesions, traumatic events, and infections are main etiologies of mandibular defects needing partial resection and bone reconstruction [93, 94]. Maintaining acceptable esthetic and functional outcomes and facial symmetry are the main goals of mandibular reconstructions. Titanium reconstruction plates are biocompatible and adaptable alloplasts for temporary

reconstructions [95]. For more reliable reconstruction, autogenous bone grafts are commonly used. Complex mandibular morphology and muscular attachments moving the jaw in unfavorable positions are challenging to oral and maxillofacial surgeons in mandibular reconstructions [23]. 3D printing technology can be used in different aspects of facial reconstruction. This technology is widely used for mandibular reconstruction [96]. Better anatomical understanding, proper plate adaptation, plate pre-bending, precise bone harvesting by utilizing negative templates of the defect, reduced bone-plate distance, decreased duration of surgery, less blood loss, and shortened duration of general anesthesia are the main advantages of using additive manufacturing in mandibular reconstruction (Figure 8) [23, 96].

Hanasono and Skorackil indicated that 3D printing can reduce surgery duration up to 1.4 hour [97].

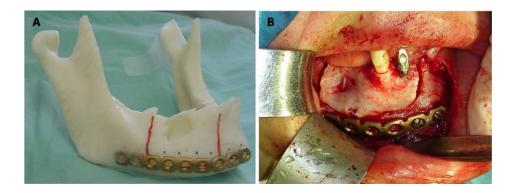


Figure 8. (a) Precontoured reconstruction plate before marginal mandibulectomy aiming to reinforce the remaining thin mandibular lower border; (b) note the anatomic alignment of the precontoured plate to the lower mandibular border [23].

#### 6. Improvements in learning, training, and practice

#### 6.1. Surgical education

Medical training can reform with enhancements of 3D printing technology [84].

As oral and maxillofacial surgeons, we are expected to master detailed morphology of the head and neck region and their spatial relationship. Patients and medical trainees and residents can benefit from 3D printed models [26, 98]. High maintenance charges, cultural and social complications, and formalin-related safety issues are making cadavers a limited source for medical education [99, 100].

Medical trainees can have better understanding of anatomical structure with 3D printed models.

These models allow a thorough and complete training before a surgery even begins [101, 102]. Operators can perform complicated surgeries on 3D models without any concerns and complications [103]. 3D printing also can aid in better understanding of patients' medical situation rather than a flat 2D screen [12]. Kah Heng Alexander et al. conducted a double blind randomized controlled trial to compare the success of 3D printing with human cadavers for distinguishing external cardiac anatomy. 3D printed models had significantly higher scores in comparison to the cadavers or combined groups [98]. With the enhancement of new materials, 3D printed models will be more accurate in the future [104–106].

#### 6.2. Patient education

Fulfilling patient expectations is critical to have successful surgical outcomes. Surgeon-patient professional relationship can be simplified using 3D printing. In preoperative consultations, patients can understand surgical details, different results, and potential obstacles. Therefore, 3D printed models can aid gaining informed consent. [103]. CT/MRI scans that we use today to explain the procedure for the patients are usually hard to understand for uneducated patients. Patients mostly do not comprehend the situation.

Literature has shown that 3D printed models result in better training of both patients and medical trainees [26, 107, 108]. Also having in-office preoperative and postoperative 3D printed models of specific surgeries can help patients justify their expectations [26].

Patients' families can also benefit from additive manufacturing since they might have positive impacts on patient satisfaction. These models could be utilized to form a library for future educational goals [109].

#### 7. Prospective visions

Three-dimensional printers are a new and emerging technology with the ability to manufacture physical objects from digital files. Decreasing hardware costs have made this technology affordable for use in the office setting [26]. 3D printing technology enables more effective patient consultations, increases diagnostic quality, improves surgical planning, acts as an orientation aid during surgical procedures, and manufactures guiding template segmental resections. In the future, additive manufacturing might be capable of organ bio-printing [30]. Surgery is a practical art! The surgeon often uses direct physical intervention in the treatment of patients. Surgical procedures must be accurately planned for each patient individually to minimize complications and increase benefits. In oral and maxillofacial surgery, potential uses extend to surgical planning, education, and prosthetic device design and development. RP is not utilized in conventional clinical applications but can revolutionize oral and maxillofacial surgery in the future [26]. To clarify and understand what is the best prediction for the future of the technology itself, production time of objects and costs should also be considered. Different researchers have indicated that they have found 3D printing a cost-effective technology [110-112]. However, some other investigators have doubted efficiency and price of RP [113]. 3D printed replicas are considered to be more precise and cost-effective for patients and trainee education compared to other techniques [114]. This method also eliminates the need for animal studies [64]. 3D printing technology is here to improve our lifestyle and health care in the twenty-first century [103].

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#### References

- [1] Gibbs DM, Vaezi M, Yang S, Oreffo RO. Hope versus hype: what can additive manufacturing realistically offer trauma and orthopedic surgery? Regenerative Medicine. 2014;9(4):535–49.
- [2] Canstein C, Cachot P, Faust A, Stalder A, Bock J, Frydrychowicz A, et al. 3D MR flow analysis in realistic rapid-prototyping model systems of the thoracic aorta: comparison with in vivo data and computational fluid dynamics in identical vessel geometries. Magnetic Resonance in Medicine. 2008;59(3):535–46.
- [3] Müller A, Krishnan KG, Uhl E, Mast G. The application of rapid prototyping techniques in cranial reconstruction and preoperative planning in neurosurgery. Journal of Craniofacial Surgery. 2003;14(6):899–914.
- [4] Hoy MB. 3D printing: making things at the library. Medical Reference Services Quarterly. 2013;32(1):93-9.
- [5] Rengier F, Mehndiratta A, von Tengg-Kobligk H, Zechmann CM, Unterhinninghofen R, Kauczor H-U, et al. 3D printing based on imaging data: review of medical applications. International Journal of Computer Assisted Radiology and Surgery. 2010;5(4): 335-41.
- [6] Chae MP, Rozen WM, McMenamin PG, Findlay MW, Spychal RT, Hunter-Smith DJ. Emerging applications of bedside 3D printing in plastic surgery. Frontiers in Surgery. 2015;2.

- [7] Mertz L. New world of 3-d printing offers "completely new ways of thinking": q&a with author, engineer, and 3-d printing expert hod lipson. IEEE Pulse. 2013;4(6):12–4.
- [8] Ibrahim AM, Jose RR, Rabie AN, Gerstle TL, Lee BT, Lin SJ. Three-dimensional printing in developing countries. Plastic and Reconstructive Surgery Global Open. 2015;3(7).
- [9] Chan HH, Siewerdsen JH, Vescan A, Daly MJ, Prisman E, Irish JC. 3D rapid prototyping for otolaryngology - head and neck surgery: applications in image-guidance, surgical simulation and patient-specific modeling. PLoS One. 2015;10(9):e0136370.
- [10] Mendez BM, Chiodo MV, Patel PA. Customized "In-Office" three-dimensional printing for virtual surgical planning in craniofacial surgery. Journal of Craniofacial Surgery. 2015;26(5):1584-6.
- [11] Cunningham LL, Madsen MJ, Peterson G. Stereolithographic modeling technology applied to tumor resection. Journal of Oral and Maxillofacial Surgery. 2005;63(6):873-8.
- [12] AlAli AB, Griffin MF, Butler PE. Three-dimensional printing surgical applications. Eplasty. 2015;15.
- [13] Hull CW. Apparatus for production of three-dimensional objects by stereolithography. Google Patents; 1986.
- [14] Dawood A, Marti BM, Sauret-Jackson V, Darwood A. 3D printing in dentistry. British Dental Journal. 2015;219(11):521-9.
- [15] Brix F, Hebbinghaus D, Meyer W. Verfahren und Vorrichtung für den Modellbau im Rahmen der orthopädischen und traumatologischen Operationsplanung. Röntgenpraxis. 1985;38:290-2.
- [16] Sinn DP, Cillo Jr JE, Miles BA. Stereolithography for craniofacial surgery. Journal of Craniofacial Surgery. 2006;17(5):869–75.
- [17] Mankovich NJ, Cheeseman AM, Stoker NG. The display of three-dimensional anatomy with stereolithographic models. Journal of Digital Imaging. 1990;3(3):200-3.
- [18] Suomalainen A, Stoor P, Mesimäki K, Kontio RK. Rapid prototyping modelling in oral and maxillofacial surgery: a two year retrospective study. Journal of Clinical and Experimental Dentistry. 2015;7(5):e605.
- [19] Barker T, Earwaker W, Lisle D. Accuracy of stereolithographic models of human anatomy. Australasian Radiology. 1994;38(2):106–11.
- [20] Frühwald J, Schicho KA, Figl M, Benesch T, Watzinger F, Kainberger F. Accuracy of craniofacial measurements: computed tomography and three-dimensional computed tomography compared with stereolithographic models. Journal of Craniofacial Surgery. 2008;19(1):22-6.

- [21] Mazzoli A, Germani M, Moriconi G. Application of optical digitizing techniques to evaluate the shape accuracy of anatomical models derived from computed tomography data. Journal of Oral and Maxillofacial Surgery. 2007;65(7):1410-8.
- [22] Mehra P, Miner J, D'Innocenzo R, Nadershah M. Use of 3-d stereolithographic models in oral and maxillofacial surgery. Journal of Maxillofacial and Oral Surgery. 2011;10(1): 6–13.
- [23] Cohen A, Laviv A, Berman P, Nashef R, Abu-Tair J. Mandibular reconstruction using stereolithographic 3-dimensional printing modeling technology. Oral Surgery, Oral Medicine, Oral Pathology, Oral Radiology, and Endodontology. 2009;108(5):661–6.
- [24] Mazzoni S, Marchetti C, Sgarzani R, Cipriani R, Scotti R, Ciocca L. Prosthetically guided maxillofacial surgery: evaluation of the accuracy of a surgical guide and custom-made bone plate in oncology patients after mandibular reconstruction. Plastic and Reconstructive Surgery. 2013;131(6):1376-85.
- [25] Eppley BL, Sadove AM. Computer-generated patient models for reconstruction of cranial and facial deformities. Journal of Craniofacial Surgery. 1998;9(6):548-56.
- [26] Gerstle TL, Ibrahim AM, Kim PS, Lee BT, Lin SJ. A plastic surgery application in evolution: three-dimensional printing. Plastic and Reconstructive Surgery. 2014;133(2): 446-51.
- [27] Chopra K, Gastman BR, Manson PN. Stereolithographic modeling in reconstructive surgery of the craniofacial skeleton after tumor resection. Plastic and Reconstructive Surgery. 2012;129(4):743e-5e.
- [28] Melchels FP, Feijen J, Grijpma DW. A review on stereolithography and its applications in biomedical engineering. Biomaterials. 2010;31(24):6121–30.
- [29] Yan X, Gu P. A review of rapid prototyping technologies and systems. Computer-Aided Design. 1996;28(4):307–18.
- [30] Choi JW, Kim N. Clinical application of three-dimensional printing technology in craniofacial plastic surgery. Archives of Plastic Surgery. 2015;42(3):267–77.
- [31] Dowler C. Automatic model building cuts design time, costs. Plastics Engineering. 1989;45(4):43-5.
- [32] Fisher JP, Dean D, Mikos AG. Photocrosslinking characteristics and mechanical properties of diethyl fumarate/poly (propylene fumarate) biomaterials. Biomaterials. 2002;23(22):4333-43.
- [33] Billiet T, Vandenhaute M, Schelfhout J, Van Vlierberghe S, Dubruel P. A review of trends and limitations in hydrogel-rapid prototyping for tissue engineering. Biomaterials. 2012;33(26):6020-41.
- [34] Rozen WM, Ting JW, Leung M, Wu T, Ying D, Leong J. Advancing image-guided surgery in microvascular mandibular reconstruction: combining bony and vascular

- imaging with computed tomography-guided stereolithographic bone modeling. Plastic and Reconstructive Surgery. 2012;130(1):227e–9e.
- [35] Rozen WM, Ting JW, Baillieu C, Leong J. Stereolithographic modeling of the deep circumflex iliac artery and its vascular branching: a further advance in computed tomography-guided flap planning. Plastic and Reconstructive Surgery. 2012;130(2): 380e-2e.
- [36] Hannen E. Recreating the original contour in tumor deformed mandibles for plate adapting. International Journal of Oral and Maxillofacial Surgery. 2006;35(2):183–5.
- [37] Ono I, Gunji H, Suda K, Kaneko F. Method for preparing an exact-size model using helical volume scan computed tomography. Plastic and Reconstructive Surgery. 1994;93(7):1363.
- [38] Chang PS-H, Parker TH, Patrick CW, Miller MJ. The accuracy of stereolithography in planning craniofacial bone replacement. Journal of Craniofacial Surgery. 2003;14(2): 164-70.
- [39] Choi J-Y, Choi J-H, Kim N-K, Kim Y, Lee J-K, Kim M-K, et al. Analysis of errors in medical rapid prototyping models. International Journal of Oral and Maxillofacial Surgery. 2002;31(1):23-32.
- [40] Chia HN, Wu BM. Recent advances in 3D printing of biomaterials. Journal of Biological Engineering. 2015;9(1):4.
- [41] Herlin C, Koppe M, Béziat J-L, Gleizal A. Rapid prototyping in craniofacial surgery: using a positioning guide after zygomatic osteotomy-a case report. Journal of Cranio-Maxillofacial Surgery. 2011;39(5):376–9.
- [42] Zhang X, Jiang X, Sun C. Micro-stereolithography of polymeric and ceramic microstructures. Sensors and Actuators A: Physical. 1999;77(2):149–56.
- [43] Krishnan S, Dawood A, Richards R, Henckel J, Hart A. A review of rapid prototyped surgical guides for patient-specific total knee replacement. Journal of Bone & Joint Surgery, British Volume. 2012;94(11):1457–61.
- [44] Fortin T, Champleboux G, Lormée J, Coudert JL. Precise dental implant placement in bone using surgical guides in conjunction with medical imaging techniques. Journal of Oral Implantology. 2000;26(4):300-3.
- [45] Flügge TV, Nelson K, Schmelzeisen R, Metzger MC. Three-dimensional plotting and printing of an implant drilling guide: simplifying guided implant surgery. Journal of Oral and Maxillofacial Surgery. 2013;71(8):1340–6.
- [46] Dikovsky D, Napadensky E. Three-dimensional printing process for producing a selfdestructible temporary structure. Google Patents; 2013.

- [47] Ohtani T, Kusumoto N, Wakabayashi K, Yamada S, Nakamura T, Kumazawa Y, et al. Application of haptic device to implant dentistry-accuracy verification of drilling into a pig bone. Dental Materials Journal. 2009;28(1):75–81.
- [48] Almquist TA, Smalley DR. Thermal stereolithography. Google Patents; 1996.
- [49] Salmi M, Paloheimo K-S, Tuomi J, Wolff J, Mäkitie A. Accuracy of medical models made by additive manufacturing (rapid manufacturing). Journal of Cranio-Maxillofacial Surgery. 2013;41(7):603-9.
- [50] Silva DN, De Oliveira MG, Meurer E, Meurer MI, da Silva JVL, Santa-Bárbara A. Dimensional error in selective laser sintering and 3D-printing of models for craniomaxillary anatomy reconstruction. Journal of Cranio-Maxillofacial Surgery. 2008;36(8): 443-9.
- [51] Lethaus B, Poort L, Böckmann R, Smeets R, Tolba R, Kessler P. Additive manufacturing for microvascular reconstruction of the mandible in 20 patients. Journal of Cranio-Maxillofacial Surgery. 2012;40(1):43–6.
- [52] Klimek L, Klein H, Schneider W, Mösges R, Schmelzer B, Voy E. Stereolithographic modelling for reconstructive head surgery. Acta Oto-rhino-laryngologica Belgica. 1992;47(3):329-34.
- [53] Swaelens B, Kruth J-P, editors. Medical applications of rapid prototyping techniques. Proceedings of the 2nd European Conference on Rapid Prototyping; 1993.
- [54] Arvier J, Barker T, Yau Y, D'Urso P, Atkinson R, McDermant G. Maxillofacial biomodelling. British Journal of Oral and Maxillofacial Surgery. 1994;32(5):276–83.
- [55] Shqaidef A, Ayoub AF, Khambay BS. How accurate are rapid prototyped (RP) final orthognathic surgical wafers? A pilot study. British Journal of Oral and Maxillofacial Surgery. 2014;52(7):609–14.
- [56] Ata N. Complete mulberry hypertrophy and conchachoanal polyp of inferior turbinate. Journal of Craniofacial Surgery. 2015;26(8):e799.
- [57] Gateno J, Xia J, Teichgraeber JF, Rosen A, Hultgren B, Vadnais T. The precision of computer-generated surgical splints. Journal of Oral and Maxillofacial Surgery. 2003;61(7):814-7.
- [58] Poukens J, Haex J, Riediger D. The use of rapid prototyping in the preoperative planning of distraction osteogenesis of the cranio-maxillofacial skeleton. Computer Aided Surgery. 2003;8(3):146-54.
- [59] Dittmann W, Bill J, Wittenberg G, Reuther J, Roosen K. Stereolithography as a new method of reconstructive surgical planning in complex osseous defects of the cranial base. Technical note. Zentralblatt für Neurochirurgie. 1994;55(4):209.

- [60] Bill JS, Reuther JF, Dittmann W, Kübler N, Meier JL, Pistner H, et al. Stereolithography in oral and maxillofacial operation planning. International Journal of Oral and Maxillofacial Surgery. 1995;24(1):98–103.
- [61] Stoker NG, Mankovich NJ, Valentino D. Stereolithographic models for surgical planning: preliminary report. Journal of Oral and Maxillofacial Surgery. 1992;50(5): 466–71.
- [62] Jacobs PF. Stereolithography and other RP&M technologies: from rapid prototyping to rapid tooling. Society of Manufacturing Engineers; 1995.
- [63] Paul F. Rapid prototyping and manufacturing, fundamentals of stereolithography. SME, Dearborn, MI; 1992;8:135-41.
- [64] Klein GT, Lu Y, Wang MY. 3D printing and neurosurgery—ready for prime time? World neurosurgery. 2013;80(3):233-5.
- [65] Olszewski R, Tranduy K, Reychler H. Innovative procedure for computer-assisted genioplasty: three-dimensional cephalometry, rapid-prototyping model and surgical splint. International Journal of Oral and Maxillofacial Surgery. 2010;39(7):721-4.
- [66] Michalski MH, Ross JS. The shape of things to come: 3D printing in medicine. JAMA. 2014;312(21):2213-4.
- [67] Fullerton JN, Frodsham GC, Day RM. 3D printing for the many, not the few. Nature Biotechnology. 2014;32(11):1086-7.
- [68] Mustafa S, Evans P, Bocca A, Patton D, Sugar A, Baxter P. Customized titanium reconstruction of post-traumatic orbital wall defects: a review of 22 cases. International Journal of Oral and Maxillofacial Surgery. 2011;40(12):1357–62.
- [69] Kozakiewicz M, Elgalal M, Piotr L, Broniarczyk-Loba A, Stefanczyk L. Treatment with individual orbital wall implants in humans-1-year ophthalmologic evaluation. Journal of Cranio-Maxillofacial Surgery. 2011;39(1):30-6.
- [70] Kozakiewicz M, Elgalal M, Loba P, Komuński P, Arkuszewski P, Broniarczyk-Loba A, et al. Clinical application of 3D pre-bent titanium implants for orbital floor fractures. Journal of Cranio-Maxillofacial Surgery. 2009;37(4):229-34.
- [71] Wolff J, Sándor GK, Pyysalo M, Miettinen A, Koivumäki A-V, Kainulainen VT. Late reconstruction of orbital and naso-orbital deformities. Oral and Maxillofacial Surgery Clinics of North America. 2013;25(4):683–95.
- [72] Tabakovic SZ, Konstantinovic VS, Radosavljevic R, Movrin D, Hadžistevic M, Hatab N. Application of computer-aided designing and rapid prototyping technologies in reconstruction of blowout fractures of the orbital floor. Journal of Craniofacial Surgery. 2015;26(5):1558-63.
- [73] Metzger MC, Hohlweg-Majert B, Schwarz U, Teschner M, Hammer B, Schmelzeisen R. Manufacturing splints for orthognathic surgery using a three-dimensional printer. Oral

- Surgery, Oral Medicine, Oral Pathology, Oral Radiology, and Endodontology. 2008;105(2):e1-7.
- [74] Wu G, Zhou B, Bi Y, Zhao Y. Selective laser sintering technology for customized fabrication of facial prostheses. The Journal of Prosthetic Dentistry. 2008;100(1):56-60.
- [75] Ciocca L, De Crescenzio F, Fantini M, Scotti R. Rehabilitation of the nose using CAD/CAM and rapid prototyping technology after ablative surgery of squamous cell carcinoma: a pilot clinical report. The International Journal of Oral & Maxillofacial Implants. 2009;25(4):808-12.
- [76] Sykes LM, Parrott AM, Owen CP, Snaddon DR. Applications of rapid prototyping technology in maxillofacial prosthetics. The International Journal of Prosthodontics. 2003;17(4):454-9.
- [77] Ciocca L, De Crescenzio F, Fantini M, Scotti R. CAD/CAM bilateral ear prostheses construction for Treacher Collins syndrome patients using laser scanning and rapid prototyping. Computer Methods in Biomechanics and Biomedical Engineering. 2010;13(3):379–86.
- [78] Xie P, Hu Z, Zhang X, Li X, Gao Z, Yuan D, et al. Application of 3-dimensional printing technology to construct an eye model for fundus viewing study. 2014.
- [79] Ciocca L, Scotti R. Oculo-facial rehabilitation after facial cancer removal: updated CAD/ CAM procedures. A pilot study. Prosthetics and Orthotics International. 2013:0309364613512368.
- [80] Fantini M, De Crescenzio F, Ciocca L. Design and rapid manufacturing of anatomical prosthesis for facial rehabilitation. International Journal on Interactive Design and Manufacturing (IJIDeM). 2013;7(1):51–62.
- [81] Tsuji M, Noguchi N, Ihara K, Yamashita Y, Shikimori M, Goto M. Fabrication of a maxillofacial prosthesis using a computer-aided design and manufacturing system. Journal of Prosthodontics. 2004;13(3):179-83.
- [82] Karayazgan-Saracoglu B, Gunay Y, Atay A. Fabrication of an auricular prosthesis using computed tomography and rapid prototyping technique. Journal of Craniofacial Surgery. 2009;20(4):1169-72.
- [83] Reisberg DJ, Habakuk SW. A history of facial and ocular prosthetics. Advances in Ophthalmic Plastic and Reconstructive Surgery. 1989;8:11–24.
- [84] Bauermeister AJ, Zuriarrain A, Newman MI. Three-dimensional printing in plastic and reconstructive surgery: a systematic review. Annals of Plastic Surgery. 2015.
- [85] Karatas MO, Cifter ED, Ozenen DO, Balik A, Tuncer EB. Manufacturing implant supported auricular prostheses by rapid prototyping techniques. European Journal of Dentistry. 2011;5(4):472.

- [86] Lindsay RW, Herberg M, Liacouras P. The use of three-dimensional digital technology and additive manufacturing to create templates for soft-tissue reconstruction. Plastic and Reconstructive Surgery. 2012;130(4):630e–2e.
- [87] Subburaj K, Nair C, Rajesh S, Meshram S, Ravi B. Rapid development of auricular prosthesis using CAD and rapid prototyping technologies. International Journal of Oral and Maxillofacial Surgery. 2007;36(10):938–43.
- [88] Liacouras P, Garnes J, Roman N, Petrich A, Grant GT. Designing and manufacturing an auricular prosthesis using computed tomography, 3-dimensional photographic imaging, and additive manufacturing: a clinical report. The Journal of Prosthetic Dentistry. 2011;105(2):78-82.
- [89] Levine JP, Patel A, Saadeh PB, Hirsch DL. Computer-aided design and manufacturing in craniomaxillofacial surgery: the new state of the art. Journal of Craniofacial Surgery. 2012;23(1):288-93.
- [90] Chen J, Zhang Z, Chen X, Zhang C, Zhang G, Xu Z. Design and manufacture of customized dental implants by using reverse engineering and selective laser melting technology. The Journal of Prosthetic Dentistry. 2014;112(5):1088–95. e1.
- [91] Xiong Y, Qian C, Sun J. Fabrication of porous titanium implants by three-dimensional printing and sintering at different temperatures. Dental Materials Journal. 2012;31(5): 815-20.
- [92] Habibovic P, Gbureck U, Doillon CJ, Bassett DC, van Blitterswijk CA, Barralet JE. Osteoconduction and osteoinduction of low-temperature 3D printed bioceramic implants. Biomaterials. 2008;29(7):944-53.
- [93] Chang Y-M, Shen Y-F, Lin H-N, Tsai AH-Y, Tsai C-Y, Wei F-C. Total reconstruction and rehabilitation with vascularized fibula graft and osseointegrated teeth implantation after segmental mandibulectomy for fibrous dysplasia. Plastic and Reconstructive Surgery. 2004;113(4):1205-8.
- [94] Chana JS, Chang Y-M, Wei F-C, Shen Y-F, Chan C-P, Lin H-N, et al. Segmental mandibulectomy and immediate free fibula osteoseptocutaneous flap reconstruction with endosteal implants: an ideal treatment method for mandibular ameloblastoma. Plastic and Reconstructive Surgery. 2004;113(1):80-7.
- [95] Futran ND, Urken ML, Buchbinder D, Moscoso JF, Biller HF. Rigid fixation of vascularized bone grafts in mandibular reconstruction. Archives of Otolaryngology-Head & Neck Surgery. 1995;121(1):70-6.
- [96] Fowell C, Edmondson S, Martin T, Praveen P. Rapid prototyping and patient-specific pre-contoured reconstruction plate for comminuted fractures of the mandible. British Journal of Oral and Maxillofacial Surgery. 2015;53(10):1035–7.

- [97] Hanasono M, Skoracki R. 117B: improving the speed and accuracy of mandibular reconstruction using preoperative virtual planning and rapid prototype modeling. Plastic and Reconstructive Surgery. 2010;125(6):80.
- [98] Lim KHA, Loo ZY, Goldie SJ, Adams JW, McMenamin PG. Use of 3D printed models in medical education: a randomized control trial comparing 3D prints versus cadaveric materials for learning external cardiac anatomy. Anatomical Sciences Education. 2015.
- [99] McMenamin PG, Quayle MR, McHenry CR, Adams JW. The production of anatomical teaching resources using three-dimensional (3D) printing technology. Anatomical Sciences Education. 2014;7(6):479–86.
- [100] Lambrecht JT, Berndt D, Schumacher R, Zehnder M. Generation of three-dimensional prototype models based on cone beam computed tomography. International Journal of Computer Assisted Radiology and Surgery. 2009;4(2):175-80.
- [101] Kalejs M, von Segesser LK. Rapid prototyping of compliant human aortic roots for assessment of valved stents. Interactive Cardiovascular and Thoracic Surgery. 2009;8(2):182–6.
- [102] Armillotta A, Bonhoeffer P, Dubini G, Ferragina S, Migliavacca F, Sala G, et al. Use of rapid prototyping models in the planning of percutaneous pulmonary valved stent implantation. Proceedings of the Institution of Mechanical Engineers, Part H: Journal of Engineering in Medicine. 2007;221(4):407–16.
- [103] Malik HH, Darwood AR, Shaunak S, Kulatilake P, Abdulrahman A, Mulki O, et al. Three-dimensional printing in surgery: a review of current surgical applications. Journal of Surgical Research. 2015;199(2):512–22.
- [104] Waran V, Narayanan V, Karuppiah R, Owen SL, Aziz T. Utility of multimaterial 3D printers in creating models with pathological entities to enhance the training experience of neurosurgeons: technical note. Journal of neurosurgery. 2014;120(2):489–92.
- [105] Biglino G, Verschueren P, Zegels R, Taylor AM, Schievano S. Rapid prototyping compliant arterial phantoms for in-vitro studies and device testing. Journal of Cardiovascular Magnetic Resonance. 2013;15(2):1–7.
- [106] Mashiko T, Otani K, Kawano R, Konno T, Kaneko N, Ito Y, et al. Development of threedimensional hollow elastic model for cerebral aneurysm clipping simulation enabling rapid and low cost prototyping. World Neurosurgery. 2013.
- [107] Way TP, Barner KE. Automatic visual to tactile translation. II. Evaluation of the TACTile image creation system. IEEE Transactions on Rehabilitation Engineering. 1997;5(1):95-105.
- [108] Suzuki M, Ogawa Y, Kawano A, Hagiwara A, Yamaguchi H, Ono H. Rapid prototyping of temporal bone for surgical training and medical education. Acta Oto-laryngologica. 2004;124(4):400-2.

- [109] Niikura T, Sugimoto M, Lee SY, Sakai Y, Nishida K, Kuroda R, et al. Tactile surgical navigation system for complex acetabular fracture surgery. Orthopedics (Online). 2014;37(4):237.
- [110] Duan B, Hockaday LA, Kang KH, Butcher JT. 3D bioprinting of heterogeneous aortic valve conduits with alginate/gelatin hydrogels. Journal of Biomedical Materials Research Part A. 2013;101(5):1255–64.
- [111] Dean D, Min K-J, Bond A. Computer aided design of large-format prefabricated cranial plates. Journal of Craniofacial Surgery. 2003;14(6):819–32.
- [112] Condino S, Carbone M, Ferrari V, Faggioni L, Peri A, Ferrari M, et al. How to build patient-specific synthetic abdominal anatomies. An innovative approach from physical toward hybrid surgical simulators. The International Journal of Medical Robotics and Computer Assisted Surgery. 2011;7(2):202–13.
- [113] Jirman R, Horák Z, Mazánek J, Řezníček J. Individual replacement of the frontal bone defect: case report. Prague Medical Report. 2009;110:79–84.
- [114] Turney BW. A new model with an anatomically accurate human renal collecting system for training in fluoroscopy-guided percutaneous nephrolithotomy access. Journal of Endourology. 2014;28(3):360–3.
- [115] van Noort R, The future of dental devices is digital. Dental Materials. 2012;28(1):3–12.
- [116] CustomPartNet. 2009 [cited 2016 21 Jan]; Available from: http://www.custompartnet.com/wu/jetted-photopolymer.
- [117] Keyhan SO. Customized lateral nasal osteotomy guide: three-dimensional printer assisted fabrication. Triple R. 2016;1(1):30–1.



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