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# Assessment of Neuroinflammation in Transferred EAE Via a Translocator Protein Ligand

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## 1. Introduction

Neuroinflammation is involved in the pathogenesis and progression of neurological disorders such as Alzheimer's disease and multiple sclerosis (MS) (Doorduyn et al., 2008). MS has been considered a T cell-mediated autoimmune disorder of the central nervous system (CNS), characterized by inflammatory cell infiltration and myelin destruction (Hauser et al., 1986) and focal demyelinated lesions in the white matter are the traditional hallmarks of MS. However more recent evidence suggests more widespread damage to the brain and spinal cord, to areas of white matter distant from the inflammatory lesions and demyelination of deep and cortical grey matter (McFarland & Martin, 2007). Experimental autoimmune encephalomyelitis (EAE) is an extensively used model of T-cell mediated CNS inflammation; modelling disease processes involved in MS. EAE can be induced in several species by immunization with myelin antigens or via adoptive transfer of myelin-reactive T cells. The models of EAE in rodents [actively induced and transferred] provide information about different phases [inflammation, demyelination and remyelination] and types [monophasic, chronic-relapsing and chronic-progressive] of the human disease multiple sclerosis and a vast amount of clinical and histopathologic data has been accumulated through the decades. A key aim of current investigations is developing the ability to recognise the early symptoms of the disease and to follow its course and response to treatment.

Molecular imaging is a rapidly evolving field of research that involves the evaluation of biochemical and physiological processes utilising specific, radioactive, fluorescent and magnetic resonance imaging probes. However, it is positron emission tomography (PET) and single photon emission computer tomography (SPECT) which, due to their exquisite sensitivity involving specifically designed radiolabelled molecules, that is leading the way in molecular imaging and has greatly enabled the non-invasive “visualisation” of many diseases in both animal models and humans. Furthermore, PET and SPECT molecular

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imaging are providing invaluable imaging data based on a biochemical-molecular biology interaction rather than from the traditional anatomical view. Increasingly, PET and SPECT radiotracers have been exploited to study or identify molecular biomarkers of disease, monitor disease progression, determining the effects of a drug on a particular pathology and assess the pharmacokinetic behaviour of pharmaceuticals *in vivo*. Significantly, these new imaging systems provide investigators with an unprecedented ability to examine and measure *in vivo* biological and pharmacological processes over time in the same animals thus reducing experimental variability, time and costs. Molecular imaging based on the radiotracer principle allows chemical processes ranging from cellular events, to cellular communication and interaction in their environment, to the organisation and function of complete tissue and organs to be studied in real time without perturbation. One of the key benefits of molecular imaging is a technique that allows longitudinal studies vital for monitoring intra-individual progression in disease, or regression with supplementary pharmacotherapies. This is key in animal models of diseases such as MS, where there is significant intra-individual variability in the disease course and severity.

Recent investigations have proposed the translocator protein (TSPO; 18 kDa), also known as the peripheral benzodiazepine receptor (PBR), as a molecular target for imaging neuroinflammation (Chen & Guilarte, 2008; Doorduyn et al., 2008; Papadopoulos et al., 2006). TSPO (18 kDa) is a multimeric protein consisting of five transmembrane helices, which, in association with a 32 kDa subunit that functions as a voltage dependent anion channel and a 30 kDa subunit that functions as an adenine nucleotide carrier forms part of a hetero-oligomeric complex (McEnery et al., 1992) responsible for cholesterol, heme and calcium transport in specific tissue. TSPO is primarily located on the outer mitochondrial membrane and is predominantly expressed in visceral organs (kidney, heart) and the steroid hormone producing cells of the adrenal cortex, testis and ovaries. In the central nervous system (CNS), TSPO is sparsely expressed under normal physiological conditions, however its expression is significantly upregulated following CNS injury (Chen et al., 2004; Papadopoulos et al., 1997; Venneti et al., 2006; Venneti, et al., 2008).

Several studies have identified activated glial cells as the cells responsible for TSPO upregulation in inflamed brain tissue, both in humans and in experimental models (Mattner et al., 2011; Myers et al., 1991a; Stephenson et al., 1995; Vowinckel et al., 1997) and the TSPO ligand [<sup>11</sup>C]-PK11195 was one of the first PET ligands used for imaging activated microglia in various neurodegenerative diseases (Venneti et al., 2006). Although [<sup>11</sup>C]-(R)-PK11195 is widely used for imaging of microglia, its considerable high plasma protein binding, high levels of nonspecific binding, relatively poor blood-brain barrier permeability and short half-life, limits its use in brain imaging (Chauveau et al., 2008). Recently, alternative PET radioligands for TSPO including the phenoxyarylacetamide derivative [<sup>11</sup>C]-DAA1106 and its analogues (Gulyas et al., 2009; Takano et al., 2010; Venneti et al., 2008), the imidazopyridines (PBR111) and its analogues (Boutin et al., 2007a; Fookes et al., 2008) and the pyrazolo[1,5-a]pyrimidine derivatives [<sup>18</sup>F]-DPA-714 and [<sup>11</sup>C]-DPA-713 (Boutin et al., 2007b; James et al., 2008) have been investigated.

In addition to imaging with PET, recent advances in new generation of hybrid SPECT imaging systems enabling increased resolution and morphological documentation with associated computed tomography have been made for use clinically and preclinically. These

advances have created a need and an opportunity for SPECT tracers; particularly those incorporating the longer lived radiotracer iodine-123 ( $t_{1/2} = 13.2$  h), to facilitate extended longitudinal imaging studies.

In this study the recently developed high-affinity TSPO, SPECT ligand, 6-chloro-2-(4'-iodophenyl)-3-(N,N-diethyl)-imidazo[1,2-a]pyridine-3-acetamide or CLINDE, was used to explore the expression of activated glia in a model of transferred EAE (tEAE). [ $^{123}\text{I}$ ]-CLINDE has demonstrated its potency and specificity for TSPO binding, its ability to penetrate the blood-brain barrier and suitable pharmacokinetics for SPECT imaging studies (Mattner et al., 2008). It has also been shown that [ $^{123}\text{I}$ ]-CLINDE was able to detect *in vivo* inflammatory processes characterized by increased density of TSPO in several animal models (Arlicot et al., 2008; Arlicot et al., 2010; Mattner et al., 2005; Mattner et al., 2011; Song et al., 2010), thus representing a promising SPECT radiotracer for imaging neuroinflammation. The present study aimed to investigate the effectiveness of [ $^{123}\text{I}$ ]-CLINDE to detect and quantify the activated glia and consequently correlate the intensity of TSPO upregulation with the severity of disease in a model of tEAE.

## **2. *In vivo* distribution and *in vitro* binding of TSPO - correlation with upregulation in a model of tEAE**

### **2.1 *In vivo* evaluation**

The effectiveness of [ $^{123}\text{I}$ ]-CLINDE to detect and quantify activated glia and correlate TSPO upregulation to the severity of neuroinflammation was assessed on a Lewis rat model of tEAE (Willenborg et al., 1986). The intravenous injection of myelin basic protein (MBP)-specific T lymphoblasts results in a single disease episode. The cells should be used when encephalitogenic, i.e. in the first three days after MBP re-stimulation of spleen or lymph node cells (from MBP- complete Freund's adjuvant (CFA) primed Lewis rats) or established MBP-specific CD4<sup>+</sup> IFN $\gamma$  producing T line cells (De Mestre et al., 2007). A huge advantage of this model of neuroinflammation is its uniform time course.

Male Lewis rats (Animal Resource Centre, Australia) were maintained and monitored according to Australian laws governing animal experimentation. The rats were immunised with emulsion of bovine MBP and CFA (4 mg/ml Mycobacterium butyricum). On day 10 the popliteal and inguinal lymph nodes were removed and single cell suspensions were incubated with the antigens MBP or PPD (50  $\mu\text{g}/\text{ml}$ ) for 3 days. MBP and PPD lymphoblasts were isolated on a density gradient ( $d=1.077$ ), propagated in IL-2 containing medium for 25 h and  $3 \times 10^7$  cells were injected via the lateral tail vein into naive Lewis rats. The rats were examined daily and a clinical score assigned according to the accepted scale: 0, asymptomatic; 1, flaccid distal half of the tail; 2, entire tail flaccid; 3, ataxia (difficulty righting). Half values were given when assessment fell between two scores.

The radiotracers [ $^{123}\text{I}$ ]-CLINDE and [ $^{125}\text{I}$ ]-CLINDE were synthesized as previously described (Katsifis et al., 2000) using an improved method, giving rise to high purity and high specific activity product. Briefly the tributyltin precursor (50-100  $\mu\text{g}$ ) in acetic acid (200  $\mu\text{L}$ ) was treated with a solution of either no carrier added Na $^{123}\text{I}$  in 0.02 M NaOH (Australian Radioisotopes and Industrials, Sydney, Australia) or Na $^{125}\text{I}$  (GE-Healthcare) followed by peracetic acid (1-3%, 100  $\mu\text{L}$ ). After 5 min the reaction was quenched (sodium bisulphite, 200  $\mu\text{L}$ , 50 mg/mL), neutralised (sodium bicarbonate, 200  $\mu\text{L}$ , 50 mg/mL) and injected onto a

semipreparative C-18 RP-HPLC column. The purification and isolation of [ $^{123}/^{125}\text{I}$ ]-CLINDE was carried out by C-18 RP-HPLC using a mixture of acetonitrile/0.1 M ammonium acetate 55:45 at a flow rate of 4 mL/min. Under these conditions, the radiotracer eluted at 25 min. The eluted product was evaporated to dryness and reconstituted in saline (0.9%) for *in vivo* pharmacological studies. For *in vitro* assays, unlabelled CLINDE was added to the [ $^{125}\text{I}$ ]-CLINDE to achieve a specific activity of 3.7 GBq/ $\mu\text{mol}$  and reconstituted in ethanol. The specific activity of [ $^{123}\text{I}$ ]-CLINDE was assumed to be greater than 185 GBq/ $\mu\text{mol}$  based on the limit of detection of the UV in the HPLC system used. The specific activity of [ $^{125}\text{I}$ ]-CLINDE was measured as 80 GBq/ $\mu\text{mol}$ , close to the theoretical specific activity of the [ $^{125}\text{I}$ ]-iodine.

In order to assess the distribution of the [ $^{123}\text{I}$ ]-CLINDE *in vivo*, rats showing different tEAE clinical scores were used: [0 (pre-clinical,  $n = 4$ ), 2 ( $n = 4$ ), 3 ( $n = 4$ ) and 0 (after recovery,  $n = 3$ )]. Rats were given PPD-lymphoblasts ( $n = 4$ ) and control naive rats ( $n = 4$ ) served as controls. The animals were injected via the tail vein with 0.70 MBq of [ $^{123}\text{I}$ ]-CLINDE in saline. Tissue samples were taken 3 h later, the radioactivity was measured with an automated gamma counter and the percent injected dose (%ID/g) was calculated by comparison with samples of standard dilutions of the initial dose.

Statistically significant increase in [ $^{123}\text{I}$ ]-CLINDE uptake was measured in brains and spinal cords of Lewis rats given MBP-specific T lymphoblasts that developed EAE with clinical scores of 2 and 3 (Figure 1). In the brain, the medulla oblongata, medulla pons, cerebellum, diencephalon, hypothalamus, hippocampus, frontal and posterior cortex were affected and the increase in [ $^{123}\text{I}$ ]-CLINDE uptake was in the range of 1.5 – 3.8 times.

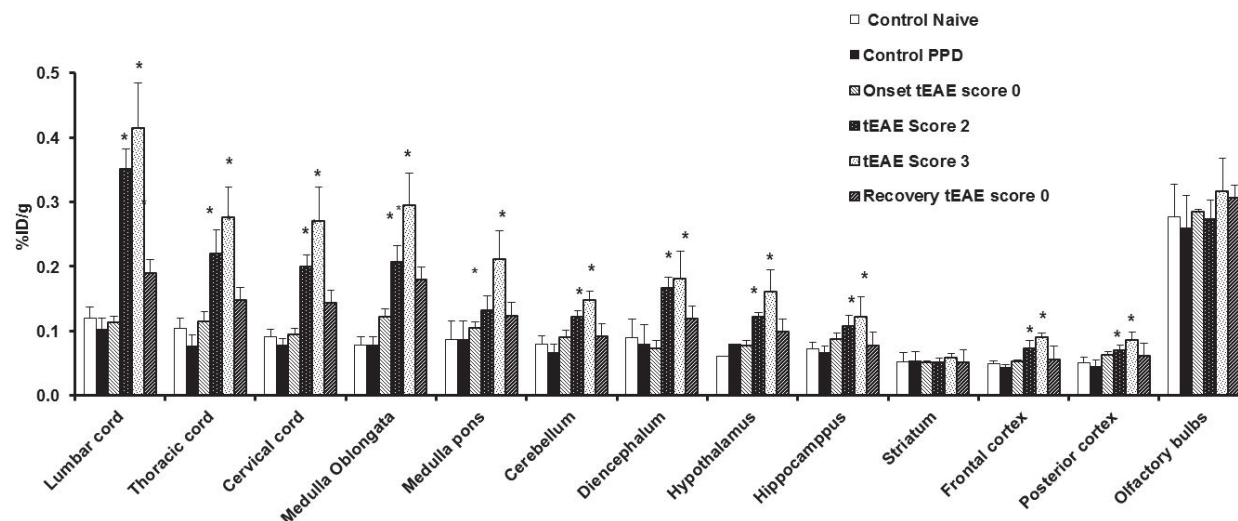


Fig. 1. Uptake of [ $^{123}\text{I}$ ]-CLINDE in the CNS. Data are represented as mean  $\pm$  SD of wet tissue.\*  $p < 0.05$  - One way ANOVA with Tukeys post-hoc test.

In the spinal cord the uptake of activity reflected the ascending nature of the inflammatory process: lumbar spinal cord > thoracic spinal cord > cervical spinal cord. The positive correlation between the ligand uptake and the disease severity is shown also in Figure 2.

Importantly, the radiotracer uptake on day 4 did not differ significantly from the one in the naive controls if the disease irrelevant PPD-specific T lymphoblasts or the disease relevant



MBP-specific T lymphoblasts were injected (Figure 1). Also, all animals showed the typical TSPO ligand biodistribution in the visceral organs and EAE severity had no influence on ligand uptake in the visceral organs (Table 1).

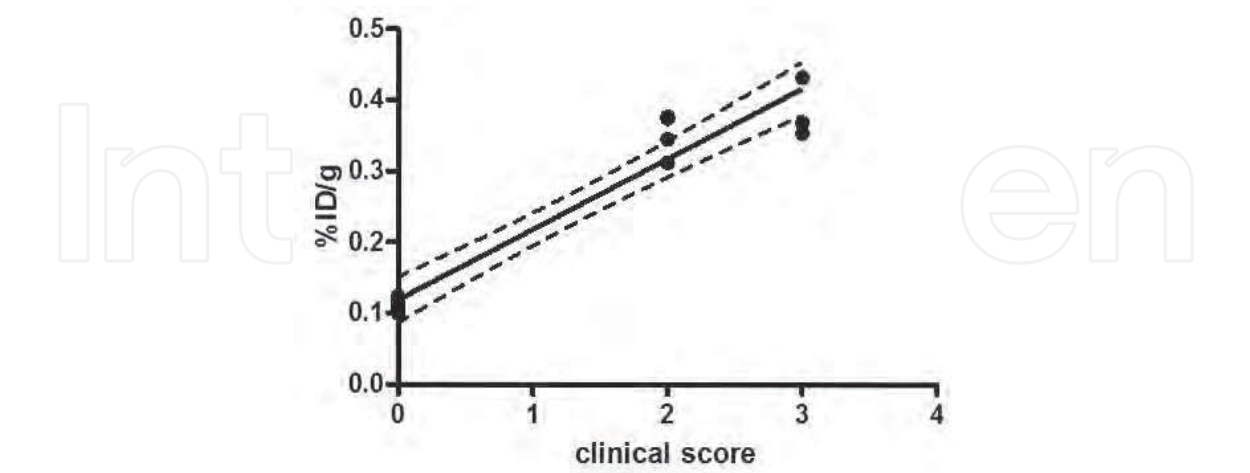


Fig. 2. Correlation between uptake of [123I]-CLINDE and disease severity in the lumbar spinal cord. Linear regression analysis, r squared value (0.97) and error bars being 95% confidence intervals for fit.

Organ	Control		tEAE			
	Naive n = 4	PDD n = 4	Score 0 Preclinical n = 4	Score 2 n = 4	Score 3 n = 4	Score 0 recovery n = 4
Liver	0.27±0.05	0.27±0.03	0.32±0.03	0.32±0.03	0.33±0.02	0.25±0.03
Spleen	3.01±0.45	3.12±0.34	3.49±0.10	3.14±0.32	3.24±0.37	3.33±0.49
Kidney	2.07±0.36	1.68±0.07	2.24±0.11	2.03±0.13	2.33±0.37	1.97±0.25
Lungs	2.27±0.41	2.01±0.18	2.41±0.32	2.12±0.16	2.27±0.38	2.05±0.24
Heart	3.24±0.49	2.85±0.29	3.81±0.14	2.87±0.08	3.16±0.31	3.32±0.03
Blood	0.04±0.01	0.04±0.01	0.06±0.00	0.04±0.01	0.05±0.01	0.04±0.00
Pancreas	0.61±0.12	0.51±0.04	0.64±0.06	0.58±0.07	0.62±0.05	0.55±0.08
Thymus	0.84±0.09	0.81±0.34	1.17±0.26	0.85±0.24	1.33±0.34	1.12±0.23
Adrenals	7.69±1.27	6.38±0.62	7.86±0.37	7.00±0.93	7.22±1.33	8.49±2.10

Table 1. Biodistribution of [123I]-CLINDE in the visceral organs of Lewis rats given MBP-specific T lymphoblasts and controls. Results are expressed as %ID/g ± SD of wet tissue

The specificity of [123I]-CLINDE binding was demonstrated in a competition study with the PK11195 (Sigma-RBI) injected in rats with tEAE clinical score 2. The *in vivo* specificity of [123I]-CLINDE was tested in two groups of four rats with tEAE clinical score 2 by injecting only [123I]-CLINDE or by injecting PK11195 (5 mg/kg) prior to [123I]-CLINDE. PK11195 was dissolved in saline with 5% dimethyl sulfoxide and injected 5 minutes prior to the injection of 0.70 MBq of the radiotracer. Animals were sacrificed 3 h p.i. and the tissues were analysed as described above.

Administration of PK11195 reduced the uptake of [ $^{123}\text{I}$ ]-CLINDE in the CNS (Figure 3) and the visceral organs with TSPO expression (data not shown) by 65-85% confirming the specificity of the ligand.

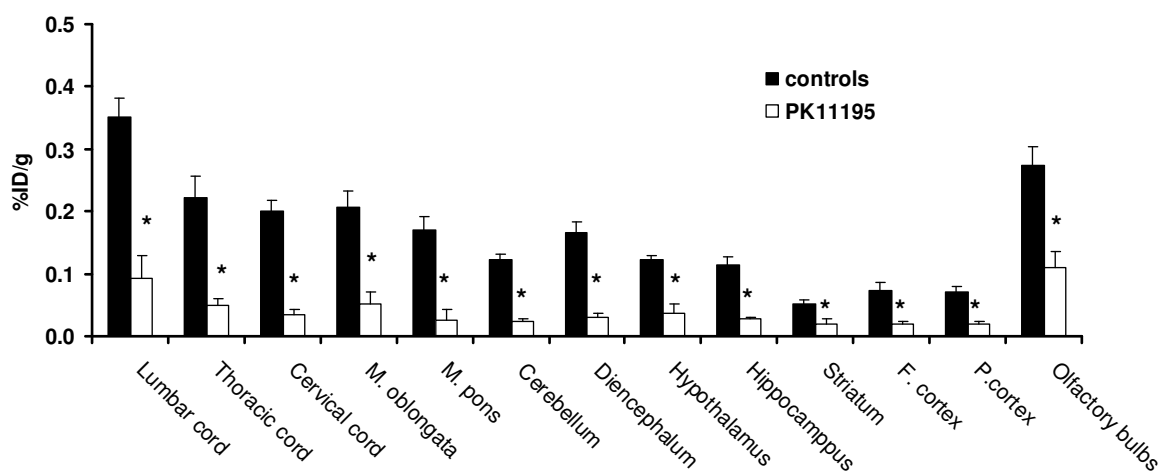


Fig. 3. Specificity of [ $^{123}\text{I}$ ]-CLINDE binding in CNS. Data are represented as mean  $\pm$  SD.

\*  $p < 0.05$  - Mann Whitney test

The feasibility of using TSPO as a marker to assess the degree of microglia activation in the living rat was tested using [ $^{123}\text{I}$ ]-CLINDE on a dedicated small animal SPECT imaging system. Longitudinal imaging studies were performed using a small animal dual-head SPECT/CT camera (Flex X-SPECT, Gamma Medica Ideas Inc.) equipped with 1 mm-aperture pinhole collimators (McElroy et al., 2002). Four rats given MBP-specific T lymphoblasts and 2 control naive animals were used. The experimental rats were imaged four times (baseline, day 4, 6 and 11 post tEAE induction), while controls were imaged twice on alternate days.

Rats were injected via the tail vein with [ $^{123}\text{I}$ ]-CLINDE (20-30 MBq in 0.1 ml saline) and anaesthetized with isoflurane (2.5%). Their heads were carefully positioned at the centre of the field-of-view, and scanned between 40 and 104 minutes after the radiotracer injection. Sixty-four 1 min-projections were collected over 360 degrees by each head, at a radius-of-rotation of 45 mm. CT scan of the rat head was then performed in order to provide anatomical landmarks for the analysis. The SPECT projections of the two heads were combined and reconstructed with an iterative cone-beam algorithm (16 subsets, 4 iterations). The reconstructed data were then scaled using calibration factors to allow the measured activity to be expressed as %ID/mL. SPECT and CT volumes were automatically fused for each of the eight scans. All CT volumes of the same rat were then manually co-registered to the first one (reference), using an image visualisation and processing software (<http://brainvisa.info>). A rat brain atlas was finally coregistered onto the reference volume and statistics derived for each Region of Interest.

The average values of [ $^{123}\text{I}$ ]-CLINDE uptake in the brain measured before the induction of tEAE (expressed as a percentage of injected dose per mL) ( $0.64 \pm 0.1\%$ ID/mL) is equivalent to the average uptake of all controls imaged during the study period ( $0.71 \pm 0.3\%$ ID/mL). The peak increase in activity is reached 6 days post immunization and the uptake depends on the clinical score of the rat. The uptake of [ $^{123}\text{I}$ ]-CLINDE, as assessed by SPECT imaging

during the course of the study, is exemplified in the hypothalamus and midbrain (Fig 4A). The spatial distribution of the activity in the brain of one typical rat over time is shown in figure 4B.

Using this small animal SPECT system we could not find statistically significant differences between intra-cerebral structures in the different groups of animals. This was probably due to the fluctuation of uptake values among animals from the same experimental group showing different tEAE scoring (Figure 4A). Moreover based on the example in Figure 4, the peak uptake in different structures of the brain differs from rat to rat depending on the tEAE score, disease severity, and therefore averaging the values for the experimental group did not reach statistical significance in the data. However the brain structures that showed an increase in uptake by SPECT imaging were the same structures where increased uptake was observed in the biodistribution studies.

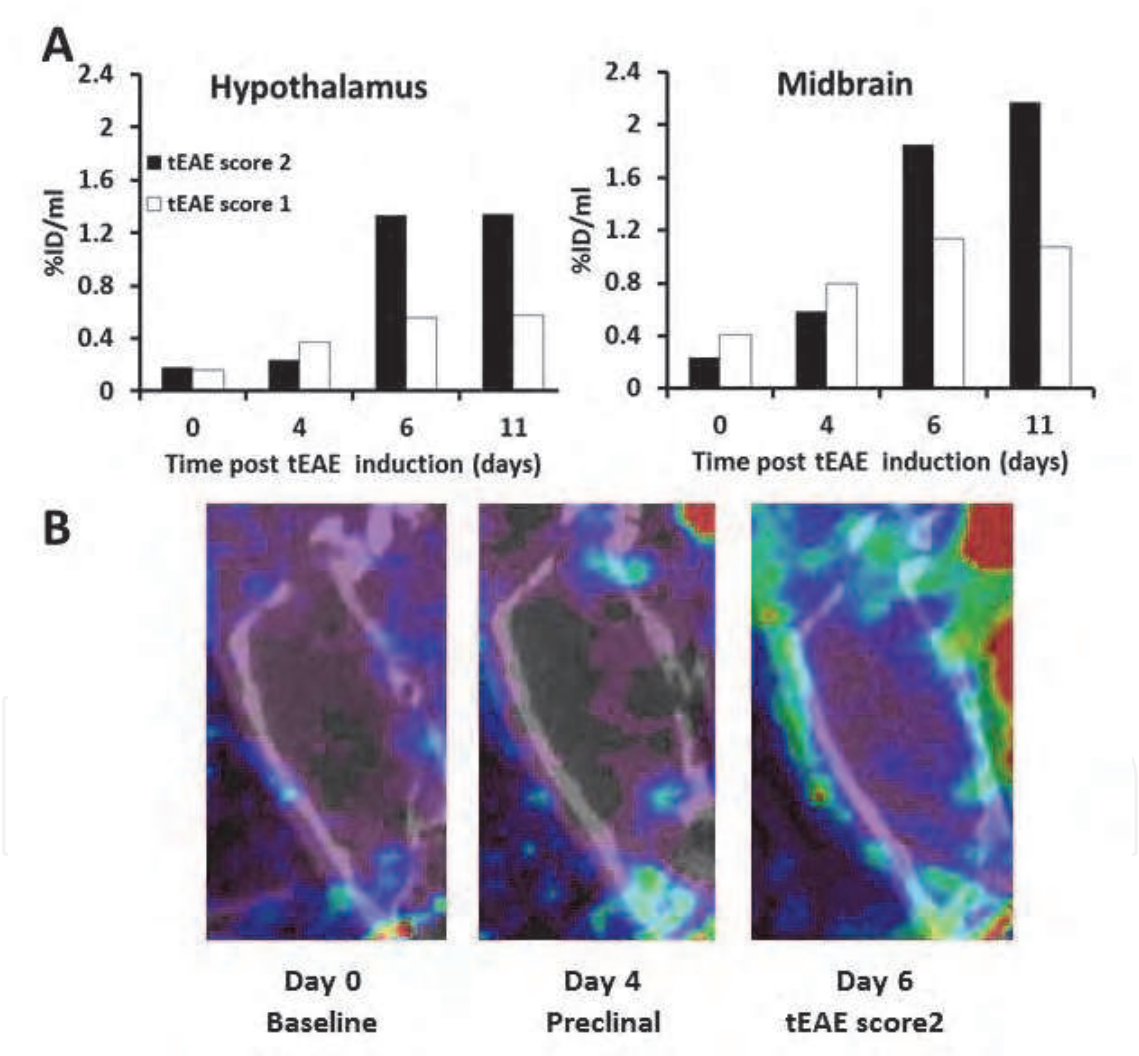


Fig. 4. *In vivo* SPECT imaging of TSPO in brain of rats given MBP-specific T lymphoblasts. **(A)** Representative individual dynamics of [<sup>123</sup>I]-CLINDE uptake in hypothalamus and midbrain (expressed as a percentage of injected dose per mL). **(B)** Representative SPECT images of [<sup>123</sup>I]-CLINDE uptake in a rat brain. The SPECT images shown were coregistered with CT at 0 (baseline), 4 and 6 days after induction of tEAE.



## 2.2 Autoradiography and immunochemistry correlation with the upregulation of TSPO in the tEAE model

*In vitro* and *ex vivo* autoradiography with [<sup>125</sup>I]-CLINDE was performed to delineate the CNS areas with TSPO uptake.

For *in vitro* autoradiography, animals with tEAE clinical scores: 2 ( $n = 3$ ) and 0 (after recovery,  $n = 5$ ) and 7 control naive rats were used. Brains and spinal cords were frozen in isopentane at  $-80^{\circ}\text{C}$ . Coronal sections (20  $\mu\text{m}$  thick) were cut, mounted onto polysine coated slides and stored at  $-20^{\circ}\text{C}$ . TSPO receptors were labeled with [<sup>125</sup>I]-CLINDE (3.7 GBq/ $\mu\text{mol}$ ) at 3 nM concentration in Tris-HCl, pH 7.4 at  $4^{\circ}\text{C}$  for 60 min. Nonspecific binding was defined by incubating adjacent tissue sections with 10  $\mu\text{M}$  of PK11195. The incubation was terminated by rinsing sections twice for 2 min in cold incubation buffer. Sections were then dipped briefly in cold distilled water and dried rapidly under a stream of cold air. The sections were affixed together with calibration standards (Amersham) to radiographic films (Amersham Hyperfilm- $\beta\text{max}$ ) for 4-6 h and developed using GBX developer and fixer (Kodak). The autoradiograms were analysed using a Microcomputer Imaging Device (MCID, Imaging research, Ontario, Canada).

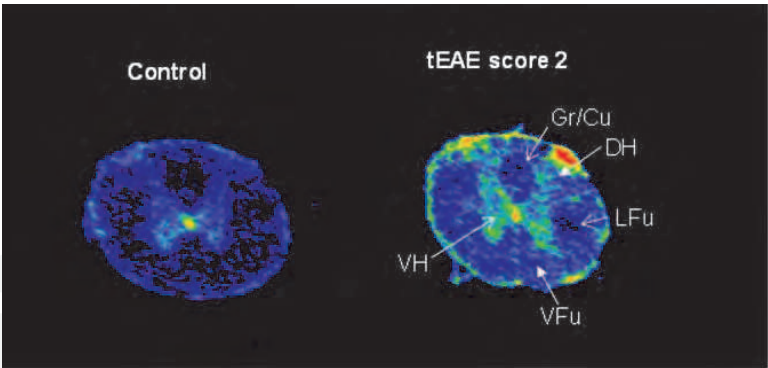
For *ex vivo* autoradiography rats with tEAE clinical scores: 3 ( $n = 3$ ) and 0 (after recovery,  $n = 3$ ) and control naive rats ( $n = 3$ ) were given [<sup>125</sup>I]-CLINDE (1.85 MBq in 100  $\mu\text{l}$  of saline) i.v. and were sacrificed 3 h after the injection of the radiotracer. Brains and spinal cords were frozen in isopentane at  $-80^{\circ}\text{C}$ . Coronal sections (20  $\mu\text{m}$  thick) were cut, thawed, dried and affixed to radiographic films (Amersham Hyperfilm- $\beta\text{max}$ ) for 10-15 days and the autoradiograms analyzed as above.

*In vitro* autoradiography with [<sup>125</sup>I]-CLINDE of the spinal cord from rats with tEAE compared to controls showed statistically significant increased binding of TSPO in areas of the grey (2 times) and white matter (1.2 - 3 times) (Figure 5). This study extends earlier observations using [<sup>3</sup>H](R)-PK11195 (Banati et al., 2000) in which increased binding in the spinal cords from rats with tEAE, at peak of clinical disease was documented.

The *in vitro* and *ex vivo* autoradiography revealed an increase in the TSPO expression at three brain levels (Figure 6), i.e. nuclear diagonal band/rostral migratory stream; substantia nigra cerebral peduncle and mammillary nucleus; ventral cochlear nucleus. Histologically, a lesion was observed in one of the five brains at level -3 mm to bregma, in the region of substantia nigra.

As the autoradiography showed a clear increase in TSPO labelling at specific regions in the forebrain, midbrain and hindbrain as well as in the spinal cord (Figures 5 and 6), immunohistochemistry was also performed in order to clarify the presence of gliosis in the TSPO positive areas.

For this purpose, brains from 2 naive rats, 2 rats given PPD-lymphoblasts (day 4), 4 rats given MBP-lymphoblasts (day 4), 3 rats tEAE score 2 and 3 rats after recovery from the episode, were fixed in formalin, placed in David Kopf Instruments (Tujunga, CA) brain blocker and cut at six levels at a distance of 2 mm. Serial 4  $\mu\text{m}$  coronal paraffin sections were taken at each of the six levels and assessed according to the rat brain atlas of Paxinos and Watson (Paxinos & Watson, 2007).



	Control	tEAE Score 2	tEAE recovery Score 0
Grey matter			
Dorsal horn (DH)	155 ± 17	365 ± 36***	236 72‡
Ventral horn (VH)	225 ± 17	225 ± 30	270 26
White matter			
Lateral funiculus (LFu)	123 ± 10	266 ± 23***	132 ± 31##
Ventral funiculus (VFu)	128 ± 14	369 ± 64***	118 ± 18##
Gracile/Cuneate Fasciculus (Gr/Cu)	117 ± 18	228 ± 7**	113 ± 17##

Fig. 5. Different cervical spinal cord TSPO expression in control rats and in rats with tEAE, using *in vitro* [<sup>125</sup>I]-CLINDE autoradiography. Results are expressed as fmol/mg T.E ± SD, *n* = 3-7, one way ANOVA with Tukeys Post Hoc test (Control vs Score 2, \*\**p*<0.01, \*\*\* *p*<0.001; Score 2 vs Recovery, ‡ *p*<0.05, ## *p*<0.01, ### *p*<0.001)

Indeed, at the level of the midbrain, in three of the four rats studied, astrogliosis was found around the lateral ventricles on day 4 after tEAE induction, i.e. just before and at the time of onset of the clinical EAE signs (Figure 7). However, with labelling for GFAP and ED-1 no changes were observed in any of the other five brain levels studied as well as in none of the six levels in three rats with tEAE score 2 and in three rats after recovery from score 2 to score 0.

The autoradiography and immunohistochemistry results confirm the immunofluorescence observations of Meeson et al (Meeson et al., 1994) indicating very little brain inflammation that is localised in the forebrain around the third ventricle. It is tempting to speculate that the change in the medial habenular nucleus and the dentate gyrus gliosis reflects a stress

reaction (Sugama et al., 2002), as this was observed around the onset of tEAE and did not persist during its development.

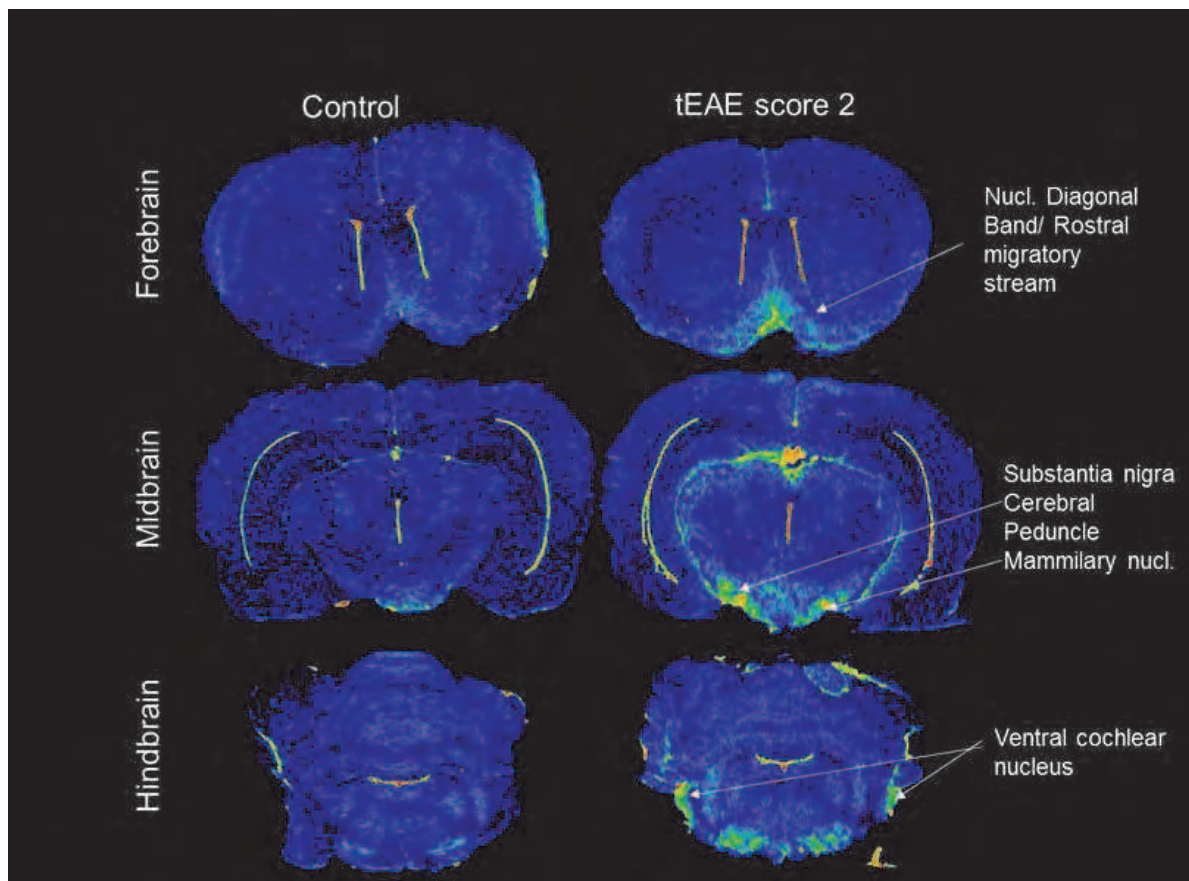


Fig. 6. Brain *in vitro* autoradiography after administration of  $[^{125}\text{I}]\text{-CLINDE}$  in Lewis rats given MBP-specific T lymphoblasts and controls

Longitudinal sections of the spinal cords were examined at the lumbar, thoracic and cervical level. After antigen retrieval (20 min boiling in citrate buffer, pH 6.0) and blocking of endogenous peroxidase and non-specific antibody binding, the macrophage/activated microglial cells were labelled with mouse anti-rat ED-1 biotin-conjugated monoclonal antibody (Serotec); TSPO - with goat polyclonal anti-TSPO IgG (Santa Cruz Biotechnology); the astrocytes - with rabbit anti-GFAP antibody (Sapphire Bioscience) and the chemokine CXCL11 - with rabbit anti-rat I-TAC IgG (kind gift from Prof. Shaun McCall, Chemokine Biology, Department of Molecular Biosciences, Adelaide University). The staining was with InnoGenex IHC Kit (San Ramon, CA) with aminoethyl carbazole (AEC) as peroxidase substrate. The sections were counterstained with Mayer's haematoxylin.

Although the histopathologic analysis and magnetic resonance (MR) microscopy had excellent correlation regarding the extent of white matter lesions on the rat EAE model (Steinbrecher et al., 2005), this imaging technology is not suitable for detection of inflammatory infiltrates in the grey matter. In our experiments significant  $[^{125}\text{I}]\text{-CLINDE}$  uptake was registered in the grey matter of the spinal cord of Lewis rats with tEAE score 2 and 3 (Figure 5). This increased uptake correlated with the positive staining for the chemokine CXCL11 that is produced mainly by astrocytes as well as with the presence of



numerous ED-1 positive cells (macrophages/glia cells) that were visualised in the spinal cord meninges and parenchyma during the tEAE episode (Figure 8). Importantly, some of these activated glial cells were positive for TSPO that supports the autoradiography quantitative data. Two days after spontaneous recovery from tEAE episode, few parenchymal cells were positive for ED-1 and there was no staining for TSPO and the chemokine CXCL11 (I-TAC).

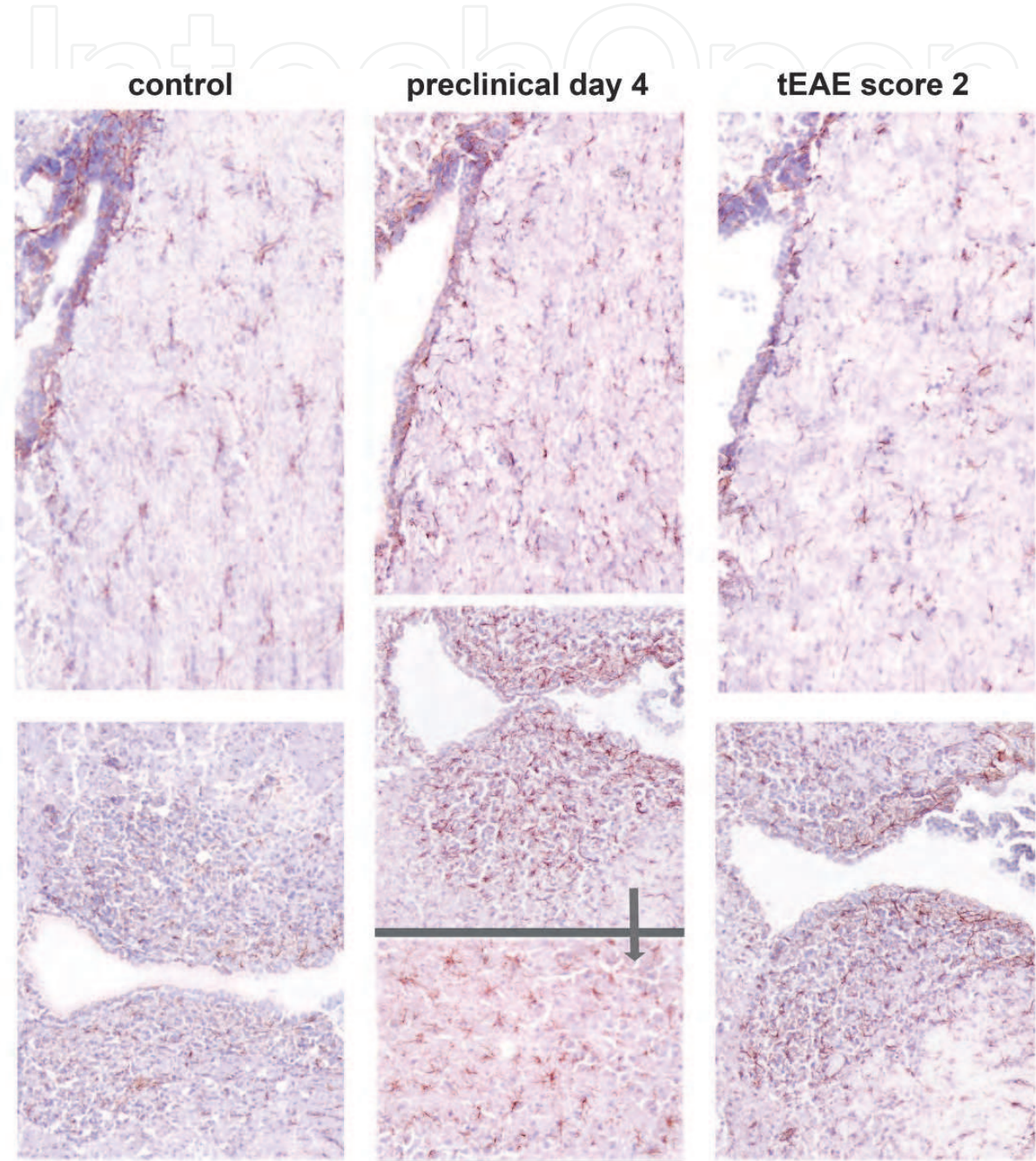


Fig. 7. Glial activation in Lewis rat tEAE (immunohistochemical evaluation). Midbrains labelled for GFAP. At disease onset, astroglyosis was observed around the 3<sup>rd</sup> ventricle in four of five animals.

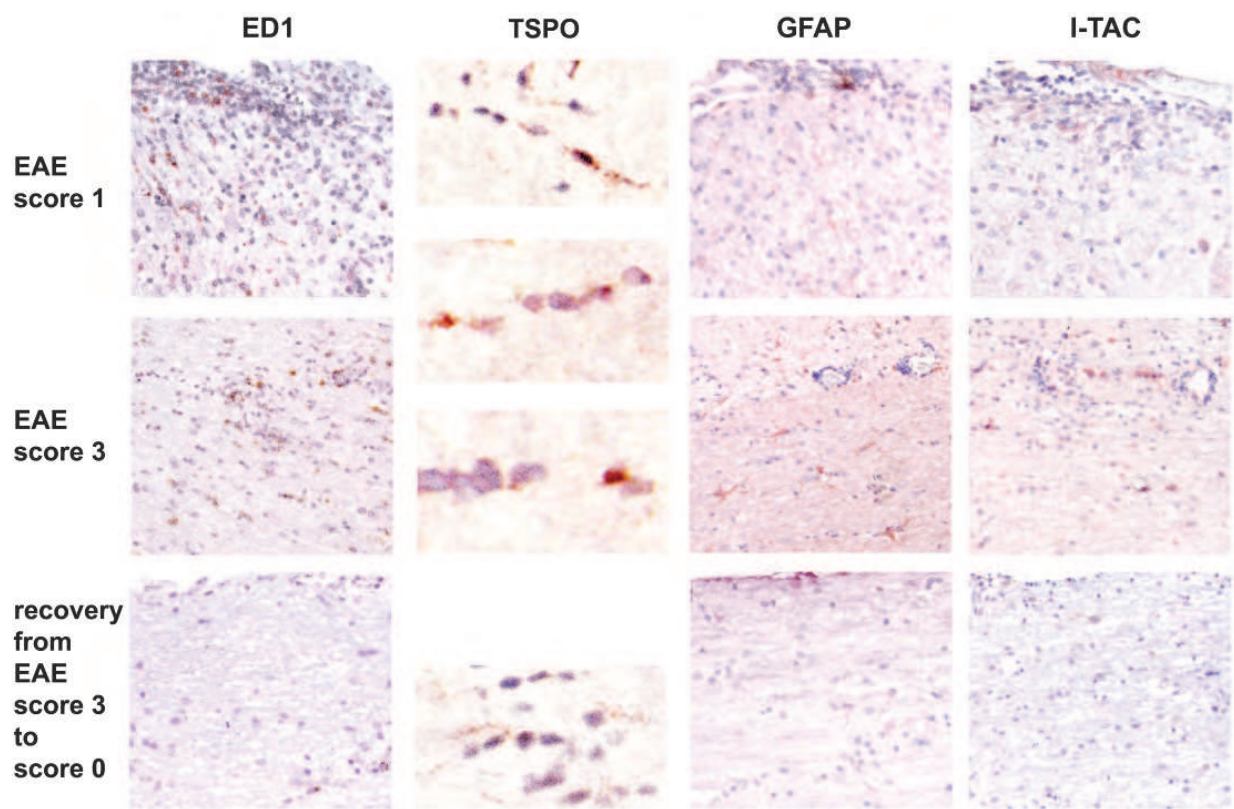


Fig. 8. Longitudinal sections of lumbar spinal cord labelled for macrophages/activated microglia (ED-1), TSPO, astrocytes and I-TAC at different clinical stages of tEAE.

One of the first *in vivo* MRI studies on tEAE in rats (Morrissey et al., 1996) showed that MRI changes were observed well before the onset of major cellular infiltration and before the onset of clinical signs that made possible to assess quantitatively the breach of the blood brain barrier (BBB) and to distinguish *in vivo* between two components of the early phase of the lesion - inflammatory infiltrates and vasogenic oedema. Increased binding of several TSPO ligands has been reported after brain injury, including focal (Myers et al., 1991a; Myers et al., 1991b) and global (Stephenson et al., 1995) cerebral ischemia in the rat where heterogeneous level of expression of TSPO in different cells is seen in the core of infarction as early as 4 days after ischemia (Rojas et al., 2007).

In this model of neuroantigen-specific neuroinflammation the significant changes were also registered from day 4 onward with SPECT imaging. A study on the same model (Banati et al., 2000) also found normal autoradiography up to day 4 with [3H]-PK11195. One should point out that we used two appropriate controls (not only naive rats). Interestingly, the time frame is similar for PET scan studies in stroke patients - the increase in binding was as early as 3 days after the onset of stroke (Price et al., 2006). Thus, any earlier *in vivo* as well as *in vitro* changes are most likely attributed to stress reaction.

The imaging studies, using the SPECT tracer [123I]-CLINDE in Lewis rat models of transferred EAE (this study) and active EAE (Mattner et al., 2005) confirm the MRI studies by other groups that the imaging changes parallel the monocyte/microglia/astrocyte activation rather than the lymphocyte infiltration (Morrissey et al., 1996; Rausch et al., 2003). These results confirm the reliability of the translocator protein (Papadopoulos &



Lecanu, 2009) in early diagnostics of antigen-specific neuroinflammation and eventually - of MS.

N.B. Discussion with mouse tEAE models was not included as they result in inflammation which progresses to demyelination (Mokhtarian et al., 1984) while the MBP-specific T lymphoblasts induced tEAE in the Lewis rat is monophasic with full recovery (Holda et al., 1980; Paterson et al., 1981).

### 3. Conclusion

Transferred EAE was induced in Lewis rats with MBP-specific T lymphoblasts and the uptake of the translocator protein (TSPO) tracer [ $^{123}\text{I}$ ]-CLINDE was studied by biodistribution, *in vitro* and *ex vivo* autoradiography, immunohistochemistry and SPECT imaging. On a background of the typical TSPO ligand biodistribution in the visceral organs, a statistically significant 2-4 fold increase was measured in brains and spinal cords of animals with EAE clinical score of 3, compared to controls (naive or given disease-irrelevant PPD-specific T-lymphoblasts). Importantly, using [ $^{123}\text{I}$ ]-CLINDE as a radiotracer we were able to register significant inflammation also in the grey matter. The CNS regional [ $^{123}\text{I}$ ]-CLINDE uptake correlated with the immunohistochemical localisation of activated glial cells. The results demonstrate the ability of this highly specific TSPO ligand to measure changes in TSPO density according to area of involvement and the severity of disease suggesting it is a useful SPECT tracer for studies on experimentally induced inflammation and in multiple sclerosis.

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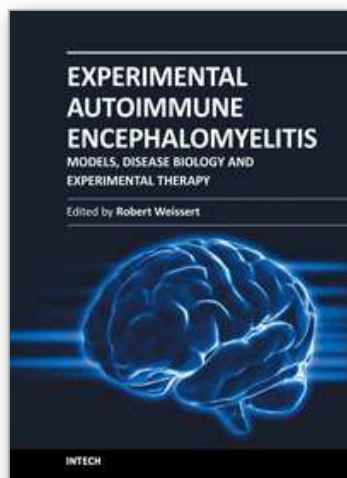
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## **Experimental Autoimmune Encephalomyelitis - Models, Disease Biology and Experimental Therapy**

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