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Monte Carlo Simulation of Pile-up Effect in Gamma Spectroscopy

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1. Introduction

As it is well known, an ideal spectroscopy amplifier should have a constant amplification for pulses of all amplitudes, without distorting any of them. Unfortunately, some pulse distortion is always present because of electronic noise, gain drift due to temperature, pulse pile-up and limitations on the linearity of the amplifier (Knoll, 2000). Therefore, the final spectrum of the detected particles in the detection system is disturbed by these factors. In this chapter, we have concentrated on pile-up effect calculation over the gamma spectrum in a NaI(Tl) scintillation detector.

The fact that pulses from a radiation detector are randomly spaced in time can lead to interfering effects between pulses, which are more likely to occur as the count rate increases. These effects are generally called pile-up. It is known that in a scintillation detector the highest possible radiation counting rate is controlled by the pulse pile-up characteristics of the detection system. In high true count rate (TCR) spectrometry, the pulse pile-up effect is considerable and its spectrum distortion can only be determined by Monte Carlo simulation. (Fazzini et al., 1995; Gostely, 1996; Tenney, 1984).

2. Background

Pile-up phenomenon is well known; it can be divided into two general types, which have somewhat different effects on pulse height measurements. The first is known as peak pile-up: it occurs when two or more pulses are sufficiently close together to be treated as a single pulse by the analysis system. The pile-up of pulses has the effect of removing them from the proper position in the pulse height spectrum, and the area under the full-energy peak in the spectrum will no longer be a true measure of the total number of full-energy events. The second type of pile-up is called tail pile-up and involves the superposition of the tail of a pulse to the next one. The effect of tail pile-up on the measurement is to worsen the energy resolution by adding wings to the shape of the recorded peaks. Since tail pile-up does not change the location of acquired events within the energy spectrum, it will not be considered in this work.

In the statistical analysis of pile-up, it is assumed that any inherent dead time of the detector and the preamplifier is small compared with the pile-up resolution time τ of the pulse

processing system. This time τ is defined as the minimum time that must separate two events to avoid pile-up. Thus, the events which arrive at the amplifier with Poisson distribution are assumed to pile-up only if they occur within a time spacing less than τ (Knoll, 2000). In this chapter we describe the Monte Carlo simulation of the pile-up effect distortion over the gamma spectrum of a NaI(Tl) detector. First, MCNP Monte Carlo code was applied to calculate the pulse height spectrum and the detector efficiency. Then, a custom code was written in FORTRAN language to simulate the distortion in pulse height spectrum due to the pile-up effect for paralyzable and nonparalyzable systems by Monte Carlo method. The results of the simulations were compared with the experimental spectra of a 137 Cs source as well as with the experimental measurement of count rate performance of a gamma camera system (Mowlavi et al., 2006).

3. Algorithm of pile-up simulation

In the statistical analysis of pile-up, it is assumed that any inherent dead time of the detector and the preamplifier is small compared with the pile-up resolution time τ of the pulse-processing system. This time τ is defined as the minimum time that must separate two events to avoid pile-up. Thus, the events which arrive at the amplifier with Poisson distribution are assumed to pile-up only if they occur within a time spacing less than τ . True events are assumed to occur at a rate n and, due to pile-up, the recording system will perceive counts at a lower rate m, so:

$$m = \frac{n}{1 + n\tau}$$
 Nonparalyzable system
 $m = ne^{-n\tau}$ Paralyzable system (1)

In general, the probability for a given count to be formed from the pile-up of (x+1) true events are (Knoll, 2000):

$$P(x) = \frac{(n\tau)^{x} e^{-n\tau}}{x!}$$
 Nonparalyzable system

$$P(x) = e^{-n\tau} (1 - e^{-n\tau})^{x}$$
 Paralyzable system (2)

Both the nonparalyzable and the paralyzable formulation have been used in pile-up simulation. The Monte Carlo calculation includes two steps, as described in the diagram of Figure 1. First, MCNP Monte Carlo code (Briesmeister, 2000) was employed to calculate the pulse height spectrum and the detector efficiency for the geometry configuration of the detection system. The simulated experimental configuration with MCNP does not take into account the actual energy resolution of the system as well as does not consider the pile-up effect. In the second step, in order to obtain a more realistic simulation, we wrote a Monte Carlo code by *FORTRAN PowerStaion 4.0* software language. The pulse height spectrum coming from the MCNP was convoluted by a Gaussian-spread function corresponding to the measured energy resolution. Then, to consider the pile-up effect, for paralyzable and nonparalyzable systems, we implemented a simulation based on Monte Carlo method. The following analytical function was applied for the pulse shape with t₀ starting time and a₀ amplitude:

$$F(t) = \begin{cases} 4a_0(1 - e^{-\frac{(t - t_0)}{\tau_p}}) & e^{-\frac{(t - t_0)}{\tau_p}} \\ 0 & t \le t_0 \end{cases}$$

$$(3)$$

where $\tau_v = 0.230 \ \mu \text{sec}$ is the time constant of NaI(Tl) crystal.

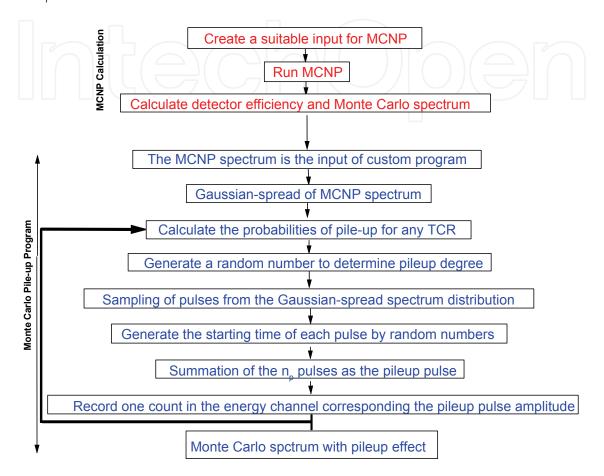


Fig. 1. The diagram of Monte Carlo pile-up calculation algorithm.

The first component of the pulse function, (1-e τ_p), corresponds to the increase of the excited states of the NaI(Tl) when the gamma radiation interacts with the crystal, and the τ_p

second component, (e $^{\tau_p}$), shows the decay of the excited states according to the exponential decay law. The summation of three pulses with different amplitude (a₀ = 5, 4, 3) and random starting time (t₀= 0.0945, 0.2854, 0.4507) are shown in Figure 2, it can be seen easily that the maximum amplitude of the pile-up pulse is 8.658.

We considered the degree of pile-up as the number of pulses n_p that made pile-up. For each true count rate (TCR), corresponding to the detector efficiency and source activity, the degree of pile-up is determined, according to the Eq. (2), by a random number (r) with uniform distribution in [0,1] interval. If r is less than P(0), one pulse is sampled from the Gaussian-spread Monte Carlo pulse height spectrum and the event is considered free of pile-up. Otherwise, if:

$$\sum_{i=0}^{k-2} P(i) < r \le \sum_{i=0}^{k-1} P(i) \tag{4}$$

 n_p pulses (n_p = k) are sampled from the Gaussian-spread Monte Carlo pulse height spectrum. After the determination of the number of pulses, the starting time of each pulse was simulated by a new random number with uniform distribution in $[0,\tau]$ interval. Finally the resulting pulse is obtained by linear superposition of the n_p pulses. We assumed the absolute maximum of the resulting pulse as its amplitude and then we recorded it in the corresponding energy channel.

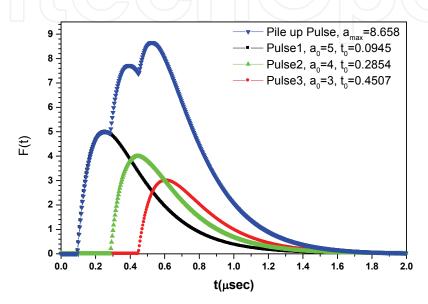


Fig. 2. The summation of the three pulses with different amplitude and random starting time.

4. Calculation of the pile-up distortion on ¹³⁷Cs pulse height spectrum

4.1 Materials and methods

We have used the pile-up code that we introduced before, to obtaine the spectrum with pile-up disturbance and the sub-spectra due to multi pulses pile-up (Mowlavi et al., 2006). Experimental spectrum of ¹³⁷Cs source has been measured by a 3in×3in NaI(Tl) scintillation detector in a lead box as shown in Fig. 3. The count rate was about 1.723 × 10⁵ per second. MCNP simulated spectrum by F8:p tally and measured spectrum are presented in Fig. 4. Differences of these spectra are clear, especially in the energy region higher than the photoelectric peak.

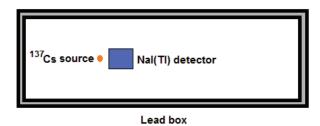


Fig. 3. The geometry set up of the ¹³⁷Cs spectrum measurement.

The MCNP pulse height output spectrum is convoluted by a Gaussian function corresponding to the energy resolution of the NaI(Tl) detector.

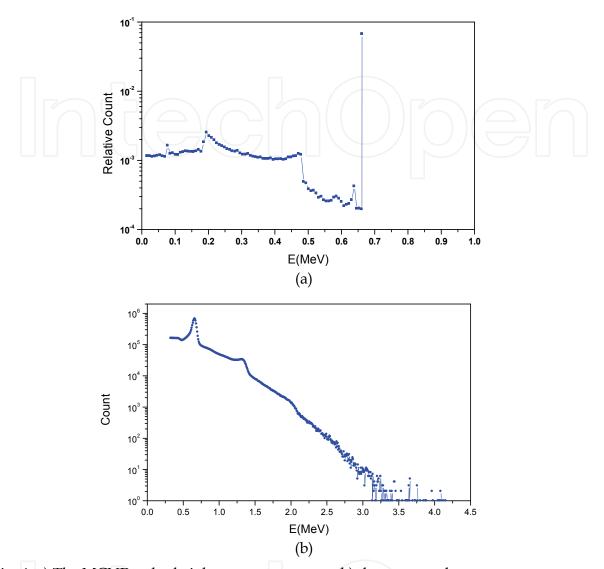


Fig. 4. a) The MCNP pulse height output spectrum; b) the measured spectrum.

4.2 Results and discussion

A comparison of experimental and pile-up computational spectra is presented in Fig. 5. The result shows a good agreement, just a little difference on the left side of photo peak at 0.662 MeV and two peak pile-up at 1.324 MeV which may be caused by tail pile-up. It can be seen the wide peak at 1.986 MeV produced by three peak pile-up. As well as, the full width at half maximum of these peaks are grown by increasing of the pile-up degree. Corresponding to the end point of the measured spectrum the pile-up occurs till sixth degree.

The total Monte Carlo spectrum together with free of pile-up, 2, 3, 4, 5 and 6 pulses pile-up sub-spectra are presented in Fig. 6. It must be mention that these sub-spectra can be obtained just by Monte Carlo simulation. About 74.77 % count in the photo peak is due to free pile-up events, 23.27% is due to two pulses pile-up, 1.88% comes from three pulses pile-up, and other portions are neglectable. It means that the main impurity under the photoelectric peak is due to two pulses pile-up.

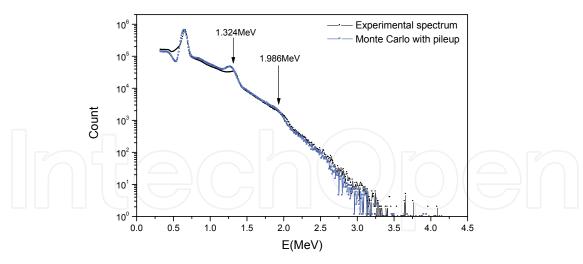


Fig. 5. Comparison of the experimental and pile-up computational spectra.

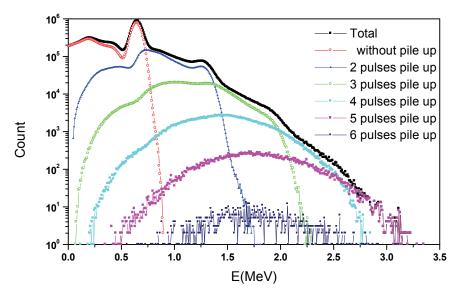


Fig. 6. The total MC spectrum together with the free of pile-up, 2, 3, 4, 5 and 6 pulses pile-up sub-spectra.

5. Monte Carlo simulation of intrinsic count rate performance of a scintillation camera

5.1 Introduction

Scintillation gamma camera is a medical equipment, therefore it must be subjected to periodical reference tests. Intrinsic count rate is considered an important parameter to be measured during the acceptance test of the instrumentation and for the periodical monitoring of the system.

The National Electrical Manufacturers Association (NEMA) and the International Atomic Energy Agency (IAEA) have published protocols for Quality Controls of Nuclear Medicine instrumentations with a detailed description of the experimental methods for the measurement of the intrinsic count rate performance (NEMA, 1994; IAEA, 1984). Based on the detailed description of the measurement procedures, it is possible to simulate the experimental condition by a Monte Carlo code analysis.

In the present work, MCNP code is used to calculate the pulse height spectrum and the gamma efficiency of a single crystal gamma camera. The simulated data so obtained are then processed by custom software to take into account the pile-up effect, a phenomenon which, at high count rate, produces a distortion in the detector spectrum which cannot be neglected.

To evaluate the consistency of the simulation, we compared the experimental measurement of intrinsic count rate performance with the Monte Carlo result.

5.2 Experimental measurement of intrinsic count rate

Intrinsic count rate test is an important measurement to evaluate the performance of a scintillation camera in terms of its response to an increasing incident gamma radiation.

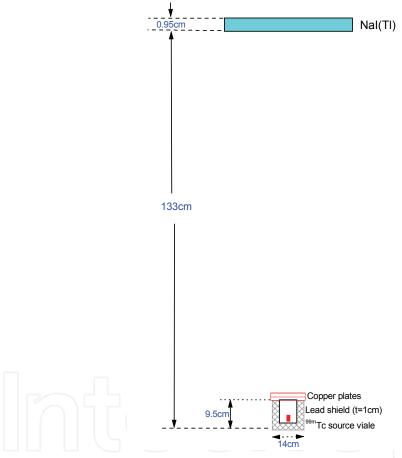


Fig. 7. The configuration of count rate test of gamma camera.

Our measurement was carried out on a gamma camera Siemens E. Cam equipped with a 9.5 mm thick NaI(Tl) single crystal detector. Following the mentioned protocols (NEMA, 1994; IAEA, 1984), we employed a ^{99m}Tc source contained in a small vial (about 10MBq) with 22 copper absorbers, each 2 mm thick, placed over the source. The gamma camera was set with a 20% window at the 140.5 keV peak. Window Observed Count Rates (WOCR) was collected for 1 minute acquisitions, starting with all the absorbers in place over the source and then removing the uppermost absorbers one by one. This procedure increases the incident gamma radiation flux and the input count rate in inverse proportion to the attenuation factor of the absorber removed. Usually calibration of absorbers is calculated by

measuring, in low count rate condition, the ratio between counts with the plate over the source and without it. In case of uniformity of the thickness of the copper plates, a mean attenuation factor \overline{A} can be used (NEMA, 1994).

For a number k of copper attenuation plates in place:

$$N(0) = A_1^{-1} A_2^{-1} A_3^{-1} \dots A_k^{-1} R(k) = R(k) \prod_{i=1}^k A_i^{-1}$$
(3)

where:

N(0)= window true count rate(WTCR) calculated for k=0 absorber plates

 A_i = individual attenuation factor of the copper plate number i

R(k) = window observed count rate(WOCR) for k plates

The configuration of the count rate test of a gamma camera has been shown in Fig. 7. Fig. 8 shows the experimental result of the count rate performance. In our measurement we evaluate the slope of the straight line of ln(WOCR) against k (number of plates over the source) in the low count rate range to determine the mean attenuation factor, \overline{A} (Geldenhuys et al., 1988).

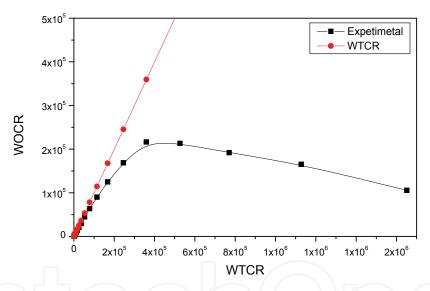


Fig. 8. The experimental result of count rate performance.

5.3 Monte Carlo simulation of intrinsic count rate performance

The Monte Carlo calculation includes two steps as describe in the diagram of Fig. 1.

First, MCNP Monte Carlo code (Briesmeister, 2000) was employed to calculate the pulse height spectrum and the detector efficiency in detecting 140.5 keV gamma rays, for a NaI(Tl) crystal and the geometrical configuration shown in Fig. 7, for various numbers of copper plates removed.

The three MCNP calculated spectra corresponding 1, 5, and 10 copper plates over the source are shown in Fig. 10-a, also Fig. 10-b shows the Gaussian spread of these spectra. It is clear that the gamma spectrum is varying with the number of copper plates over the source. Fig. 11 shows the total count per on particle from the source against the number of copper plates over the source.

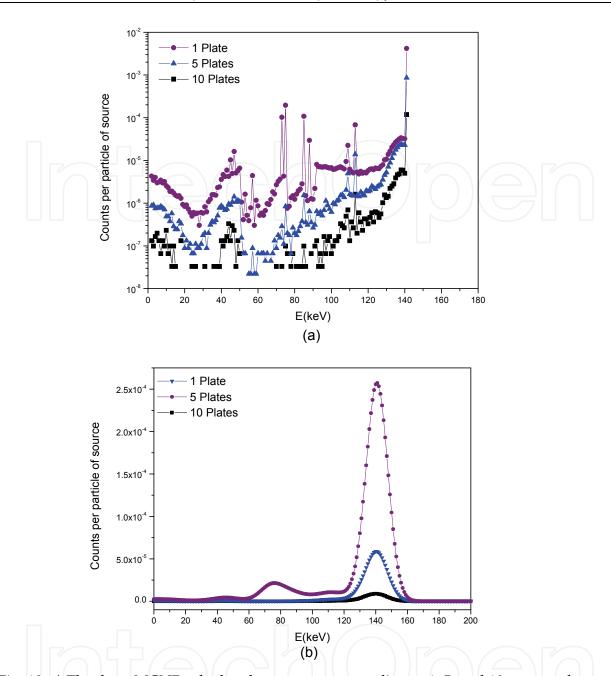


Fig. 10. a) The three MCNP calculated spectra corresponding to 1, 5, and 10 copper plates over the source, b) the Gaussian spread of the spectra.

The simulated experimental configuration with MCNP does not take into account the actual energy resolution of the system as well as does not consider the pile-up effect.

In the second step, in order to obtain a more realistic simulation, we used the Monte Carlo pile-up code. First the pulse height spectrum coming from the MCNP was convoluted by a Gaussian-spread function corresponding to the measured 11.2% gamma camera energy resolution. Fig. 12 shows the experimental spectrum of the gamma camera crystal with 11.2% energy resolution at 140.5 keV peak. Then, to consider the pile-up effect, for paralyzable and nonparalyzable systems, we implemented a simulation based on Monte Carlo method. In the next section, Monte Carlo simulation has been done for τ = 0.5, 1, 1.5 µsec values.

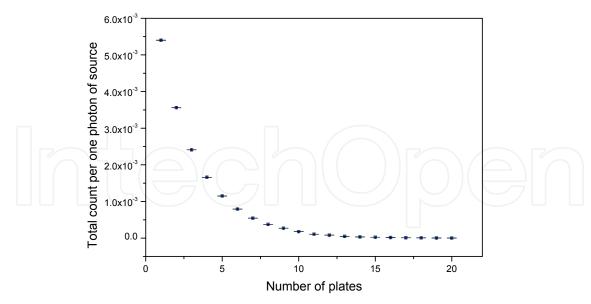


Fig. 11. The total count per one particle from the source against the number of copper plates over the source.

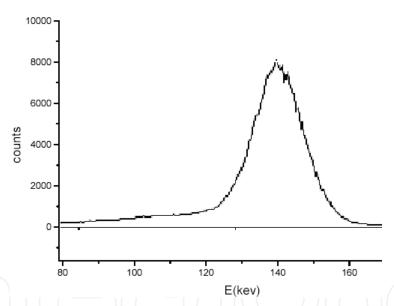


Fig. 12. The experimental spectrum of the gamma camera crystal at low count rate for a ^{99m}Tc source.

5.4 Results and discussion

We recorded the MCNP result of the detector efficiency (R) in the second column of Table 1. The third column shows the activity of 99m Tc source (A_n) in the count rate test measurement. We have calculated the pulse height spectrum without pile-up in very low count rate TCR=1, and the pulse height spectrum with pile-up in TCR=R×A_n, for any number of plates. The window observed count rate is the counts in the 20% window considering the pulse height spectrum with pile-up and the window true count rate is the counts in the 20% window considering the pulse height spectrum without pile-up (Table 1, columns 5, 6 and 7).

No. of	R	A_n	TCR	WTCR	WOCR	WOCR
Plates	(%)	(Bq)	(k count)	(k count)	Paralyzable	Nonparalyzable
	, ,			, ,	(k count)	(k count)
1	0.540±0.001	3,65E8	1969.56±1.40	1581.94±1.26	77.26±0.28	178.43±0.42
2	0.357±0.001	3,69E8	1315.26±1.14	1124.16±1.06	162.17±0.40	216.88±0.47
3	0.241±0.001	3,69E8	890.32±0.94	777.46±0.88	194.36±0.44	227.23±0.48
4	0.166±0.001	3,70E8	613.12±0.78	541.34±0.74	209.24±0.46	220.92±0.47
5	0.115±0.001	3,71E8	425.52±0.65	371.88±0.61	200.71±0.45	209.83±0.46
6	0.079±0.001	3,72E8	294.77±0.54	259.73±0.51	160.99±0.40	172.60±0.42
7	0.055±0.001	3,73E8	203.21±0.45	178.81±0.42	125.65±0.34	127.51±0.36
8	0.037±0.001	3,742E8	139.74±0.34	123.98±0.35	96.64±0.31	97.38±0.31
9	0.027±0.001	3,75E8	99.84±0.32	87.20±0.30	76.49±0.28	76.96±0.28
10	0.018±0.001	3,75E8	66.76±0.26	56.96±0.24	50.75±0.23	50.83±0.23
12	0.0082±0.0001	3,78E8	31.16±0.18	27.37±0.17	25.30±0.16	25.46±0.16
15	0.0026±0.0001	3,81E8	10.02±0.10	8.37±0.09	8.00±0.09	8.10±0.09
20	0.0004±0.0001	3,86E8	1.47±0.04	1.24±0.03	1.13±0.03	1.14±0.03

Table 1. Simulation results for count rate performance.

Fig. 13 shows the Monte Carlo spectrums without pile-up effect and with pile-up effect in paralyzable and nonparalyzable detection systems for 3 copper plates. We like to note that in high TCR, the rate of pulses that escape from the energy window due to the pile-up is higher than the WOCR. For example, in paralyzable system, with tree copper plates, the number of pulses per second which, due to the pile-up escape from the energy window is 3.07 times WOCR. Also, the contribution in WOCR from the pile-up coming from pulses with energies lower than the window interval is negligible. In nonparalyzable system, in the same condition, the number of pulses per second that escape from the energy window due to the pile-up is 2.46 times WOCR and the count rate in the energy window due to the pile-up of low energy pulses is negligible. So, in high TCR, for both paralyzable and nonparalyzable systems, the effect of pulse escaping from the window is more important than the increase of background due to the low energy pulse pile-up.

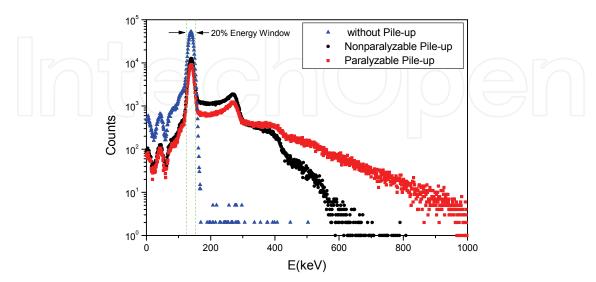


Fig. 13. The MC pulse height spectrum for three copper plates without and with pile-up in both modes.

In Fig. 14 it is reported the comparison of the pile-up defect in paralyzable and nonparalyzable systems and the sub-spectra of increasing number of pulse pile-up. In order to fund a good selection value for τ , we have done the count rate performance simulation for three values: τ =0.5, 1, 1.5 µsec. Fig. 15 shows the Monte Carlo and the experimental result of count rate performance.

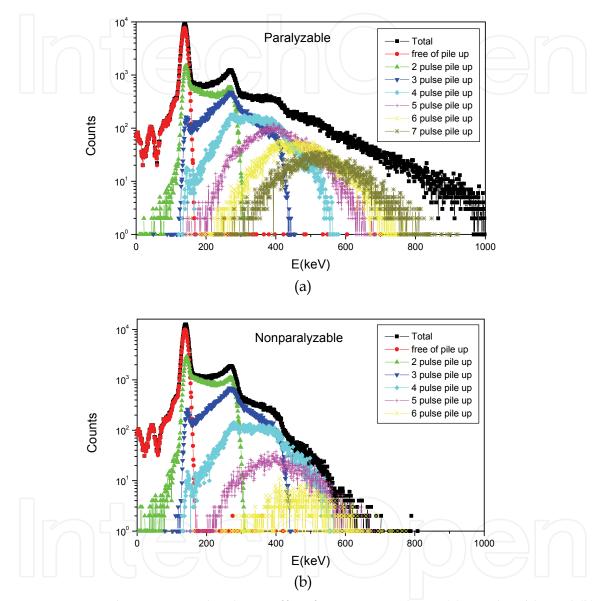


Fig. 14. Monte Carlo spectra with pile-up effect for 3 copper plates, (a) paralyzable and (b) nonparalyzable systems. Sub-spectra of subsequent pile-up pulses are also included.

The comparison of Monte Carlo and experimental results guides us to conclude that the Monte Carlo result for τ around 1 µsec is in good agreement with the experimental result for paralyzable mode. In fact, we have calculated the results for τ =0.70, 0.75, 0.80 µsec in paralayzable mode as shown in Fig. 16; and the best agreement obtained is for τ =0.75 µsec (see Fig. 17). If we consider the nonparalyzable mode for the detection system, the results show a not bad agreement for τ =2.5 µsec, although around the peak of WOCT the difference between experimental and computational data is considerable in this mode.

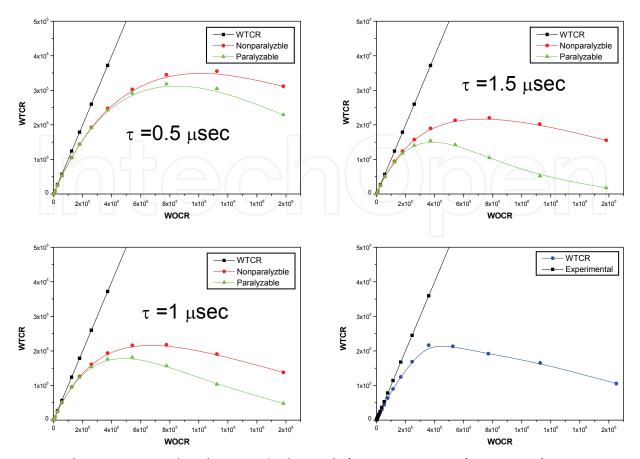


Fig. 15. The experimental and Monte Carlo result for count rate performance of nonparalyzable and paralyzable systems (all of results are shown in the same scale).

Finally, we must mention that the method can also be employed for other detectors and other counting systems (Sjöland et al., 1999; Wu et al., 1996), because it is easily customizable simply substituting some input parameters.

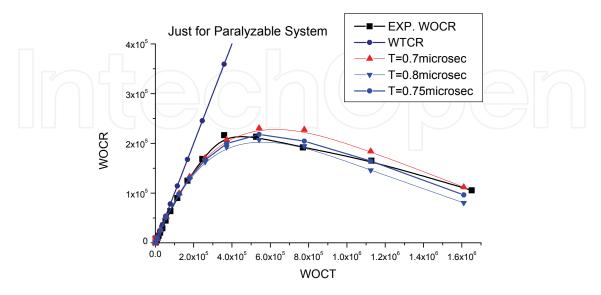


Fig. 16. The experimental and Monte Carlo result for paralyzable mode and τ =0.70, 0.75, 0.80 µsec.

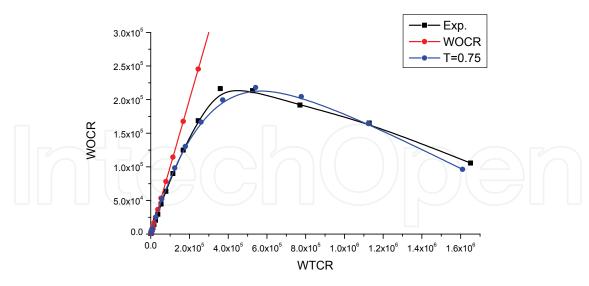


Fig. 17. The best agreement between the experimental and Monte Carlo result for paralyzable mode and τ =0.75 µsec.

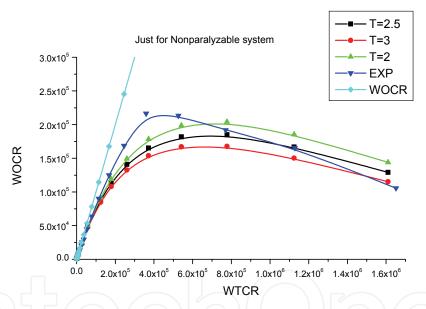


Fig. 18. The experimental and Monte Carlo result for nonparalyzable mode and τ =2, 2.5, 3 µsec.

6. Conclusion

The Monte Carlo pile-up code that we developed can be used to correct pile-up distortion in gamma spectroscopy.

At the first, we have compared and analyzed the experimental and computational spectrum considering pile-up effect of a ¹³⁷Cs source in a NaI(Tl) detector. The interesting sub-spectra have been obtained, which construct the MC spectrum with pile-up disturbance. The results have shown that the main background in the photoelectric peak is due to two pulses pile-up, about 23.27% of counts. In high count rate situation the total count of the photoelectric peak reduces effectively due to removal of pulses by pile-up.

The second application of the pile-up code was used for gamma camera count rate performance test. The Monte Carlo simulation demonstrated that the gamma camera we tested behaves in presence of a high true count rate as a paralyzable system rather than as a nonparalyzable system. In low true count rate, paralyzable and nonparalyzable simulation results are close to each other. The result obtained by simulation of pile-up with this approach showed a good agreement with experimental measurement. As a future step, we plan to apply the code on the gamma spectrum of a Prompt Gamma Neutron Activation Analysis (PGNAA) system.

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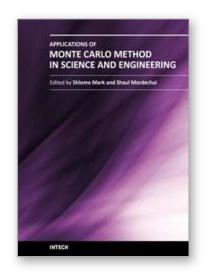
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Applications of Monte Carlo Method in Science and Engineering

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In this book, Applications of Monte Carlo Method in Science and Engineering, we further expose the broad range of applications of Monte Carlo simulation in the fields of Quantum Physics, Statistical Physics, Reliability, Medical Physics, Polycrystalline Materials, Ising Model, Chemistry, Agriculture, Food Processing, X-ray Imaging, Electron Dynamics in Doped Semiconductors, Metallurgy, Remote Sensing and much more diverse topics. The book chapters included in this volume clearly reflect the current scientific importance of Monte Carlo techniques in various fields of research.

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